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ASSESSMENT PROCEDURE

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Assessing walking adaptability in stroke patients

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ABSTRACT

Purpose: The ability to adapt walking is important for safe ambulation. Assessments of impairments in walking adaptability with the Interactive Walkway may aid in the development of individualized therapy strategies of stroke patients. The Interactive Walkway is an overground walkway with Kinect v2 sensors for a markerless registration of full-body kinematics, which can be augmented with (gait-dependent) visual context to assess walking adaptability. This study aims to evaluate the potential of the Interactive Walkway as a new technology for assessing walking adaptability in stroke patients.

Materials and methods: 30 stroke patients and 30 controls performed clinical tests, quantitative gait assessments and various walking-adaptability tasks on the Interactive Walkway. Outcome measures were compared between stroke patients and controls to examine known-groups validity. Pearson's correlation coefficients were calculated to assess the relationship between walking-adaptability outcomes and commonly used clinical test scores of walking ability and spatiotemporal gait parameters of unconstrained walking.

Results: Good known-groups validity for walking-adaptability outcomes was demonstrated. In addition, the vast majority of walking-adaptability outcomes did not or only moderately correlate with clinical test scores of walking ability and unconstrained walking parameters.

Conclusion: Interactive Walkway walking-adaptability outcomes have good known-groups validity and complement standard clinical tests and spatiotemporal gait parameters.

- ► IMPLICATIONS FOR REHABILITATION
- The Interactive Walkway allows for a comprehensive walking-adaptability assessment.
- Good known-groups validity for walking-adaptability tasks was demonstrated and walking-adaptability tasks complemented clinical tests and gait parameters.
- The Interactive Walkway has potential for monitoring recovery of walking after stroke.
- Assessments of walking adaptability may contribute to individualized interventions.

Introduction

Walking adaptability is essential for safe and independent ambulation [1]. It is defined as the ability to adapt walking to meet behavioral task goals and demands of the environment [1] and includes, among others, the ability to avoid obstacles, make sudden stops, place feet accurately in a cluttered environment and walk while performing a dual task [1]. Laboratory studies showed that stroke patients generally have a reduced ability to adapt walking to environmental circumstances [2-5]. This reduced walking adaptability makes these patients more susceptible to walking-related falls due to trips, slips or misplaced steps [6-8]. Assessing walking adaptability thus seems essential to better understand and treat walking limitations. Unfortunately, there is no comprehensive clinical test of walking adaptability [1] and laboratory studies have thus far typically focused on specific aspects of walking adaptability, mainly obstacle avoidance [2-5,9,10].

The Interactive Walkway (Figure 1) may help fill this void. It is an overground walkway equipped with multiple Kinect v2 sensors for markerless 3D full-body motion registration [11], from which spatiotemporal gait parameters can be derived. The Interactive Walkway is augmented with projected (gait-dependent) visual context, such as suddenly appearing obstacles and stop cues (based on real-time processed gait data), to assess walking adaptability [12]. Furthermore, attention-demanding secondary tasks, such as serial-3 subtractions [10] or an auditory Stroop task [3,9], can be added to assess dual-task walking.

The aim of this study is to evaluate the potential of the Interactive Walkway as a new technology for assessing walking adaptability in stroke patients. To this end, we will (1) evaluate the known-groups validity of Interactive Walkway outcome measures by comparing them between stroke patients and controls, and (2) relate these outcome measures to commonly used clinical test scores for walking ability and spatiotemporal gait parameters of unconstrained walking; considering the Interactive Walkway's strong focus on walking adaptability rather than general walking ability, we expected no or only moderate correlations.

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This article has been corrected with minor changes. These changes do not impact the academic content of the article.

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Figure 1. The set-up of the Interactive Walkway with various walking adaptability tasks (insets).

Table 1.	. In-	and	exclusion	criteria	for	stroke	patients	and	controls
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	Stroke	Control			
Inclusion criteria	 18 years or older Command of the Dutch language Experience residual motor dysfunction (Fugl-Meyer Assessment lower extremity score <34) Able to stand unsupported for more than 20 s and walk independently 	 18 years or older Command of the Dutch language Unimpaired gait Normal cognitive function (Montreal Cognitive Assessment score ≥23; [13]) Normal or corrected to normal vision 			
Exclusion criteria	 Additional neurological diseases and/or other problems interfering with gait function Less than 12 weeks post-stroke. 	 Neurological diseases and/or other problems interfering with gait function 			

Materials and methods

Subjects

Stroke patients were recruited from the outpatient clinic of the Leiden University Medical Center and from a list of patients who were discharged from the Rijnlands Rehabilitation Center. Controls were recruited *via* advertisement. In- and exclusion criteria are presented in Table 1, and differed between groups. Data was collected within the Technology in Motion project (protocol registered as NL54281.058.15; http://www.ccmo.nl/nl/ccmo-register). All subjects gave written informed consent, and the study was approved by the local medical ethics committee (P15.232).

Clinical tests for assessing walking ability

Two gait tests were included: the Timed-Up-and-Go test [14,15] and the 10-m walking test at comfortable and maximum walking speed [15,16]. Longer completion times indicate a poorer walking ability. The Tinetti Balance Assessment [17,18] has two sections that evaluate gait and balance performance, of which the combined score was used in this study (possible range 0–28; higher scores indicate better performance). Two balance tests were administered (with higher

scores indicating a better balance): the 7-item Berg Balance Scale [19], to measure static and dynamic balance during specific movement tasks (possible range 0–14), and the Functional Reach Test [20,21], to determine the maximal distance one can reach forward from a standing position.

The Interactive Walkway to quantify unconstrained walking and to assess walking adaptability

Unconstrained walking and walking adaptability were assessed on the Interactive Walkway (Figure 1; Supplementary file S1). The Interactive Walkway comprised four spatially and temporally integrated Kinect v2 sensors with optimized inter-sensor distances [22], providing markerless 3D full-body kinematics of various body points (e.g., ankles, spine base and spine shoulder). The Interactive Walkway was further equipped with a projector (EPSON EB-585W, ultra-shortthrow 3LCD projector) to augment the entire 8-m walkway with visual context for the walking-adaptability tasks. The coordinate systems of the sensors and projector were spatially aligned to a common coordinate system using a spatial calibration grid. Interactive Walkway data was sampled at 30 Hz using custom-written software utilizing the Kinect-for-Windows Software Development Kit (SDK 2.0)



Figure 2. Schematics of unconstrained walking and walking adaptability tasks on the Interactive Walkway. The available response distance of the suddenly appearing obstacles and cues varied over subjects depending on their own gait characteristics.

and recently validated for unconstrained walking and walking adaptability assessments [11,12].

Subjects performed unconstrained walking and various walking-adaptability tasks on the Interactive Walkway (Figure 2; see Table 2 for more details and Supplementary video S1 for a video of the tasks). Unconstrained walking was assessed with an 8-m walking test. Walking adaptability was assessed with the following tasks: obstacle avoidance, sudden stops-and-starts, goal-directed stepping (with symmetric and irregular stepping stones), narrow walkway, speed adjustments (speeding up and slowing down), slalom, turning (half and full turns in both directions) and dual-task walking (plain and augmented). The Interactive Walkway assessment comprised a total of 35 trials. Table 2 details the number of trials per task and their difficulty level. Dual-task walking was assessed by adding an auditory Stroop task [23] in which the words high and low (in Dutch) were pronounced at a high or low pitch (i.e., congruent and

incongruent stimuli) to both the plain 8-m walking test and the augmented obstacle-avoidance task, respectively. The subject had to respond with the pitch of the spoken word. All Interactive Walkway tasks were performed at a self-selected walking speed.

Procedure

Half of the subjects started with the block of clinical tests, the other half with the Interactive Walkway assessment. For the Interactive Walkway, every participant had a different order of the tests to prevent systematic order effects. However, the 8MWT was always performed first, which enabled us to adjust the settings of the walking-adaptability tasks to one's own gait characteristics in an attempt to obtain a similar level of difficulty for each subject (see Table 2). For example, available response times for suddenly appearing obstacles were controlled by self-selected walking

Table 2. Interactive Walkway tasks and outcome measures.

Tasks	# Trials	Level of difficulty	Characteristics	Outcome measure	Unit	Calculation
Unconstrained walking 8-m walking test	2		Walking at self-selected walking speed.	Walking speed	cm/s	The distance travelled between the 0-m and 8-m line on the walkway divided by the time, using the data
				Step length	cm	of the spine shoulder. The median of the differences in the anterior-posterior direction of
				Stride length	cm	consecutive step locations. The median of the differences in anterior-posterior direction of
				Step width	cm	Consecutive ipsilateral step locations. The median of the absolute mediolateral difference of
				Cadence	steps/min	Calculated from the number of steps in the time interval between the first and last estimate of foot contact
				Step time	S	The median of the time interval between two consecutive instants of foot contact
				Stride time	S	The median of the time interval between two consecutive ipsilateral instants of foot contact.
				Symmetry step length	%	Smallest step length (i.e., left or right) divided by the largest step length times 100%.
				Symmetry step time	%	Shortest step time (i.e., left or right) divided by the longest step time times 100%.
Walking adaptability Obstacle avoidance	5	$\begin{array}{l} \text{ART}=1\text{s} \mbox{ (three trials)} \\ \text{ART}=0.75\text{s} \mbox{ (two trials)} \end{array}$	Avoiding suddenly appearing obstacles.	Obstacle- avoidance margins	cm	The distance of the anterior shoe edge (trailing limb) and posterior shoe edge (leading limb) of the step locations to corresponding obstacle borders during obstacle crossing
				Success rate	%	Number of successfully avoided obstacles divided by the number of obstacles presented times 100%.
Sudden stops- and-starts	5	ART = 1 s (three trials) ART = 0.75 s (two trials)	Stopping behind the suddenly appearing stop cues and start	Sudden- stop margins	cm	The minimum distance of the anterior shoe edge to the corresponding stop cue border during the period in which the cue was visible
			the cues disappear.	Success rate	%	Number of successful stops divided by the number of stop cues presented times 100%
				Initiation time	S	The time between disappearance of the stop cue and the moment of first foot contact.
Goal-directed SSS stepping	3 2	Average SL 75% average SL 125% average SL 25% variation in SL left and right 50% variation in SL left and right	Stepping as accurately as possible onto the shoe-size-matched stepping stones.	Stepping accuracy	cm	The standard deviation over the signed deviations between the center of the stepping target and the center of the foot at corresponding step locations. The center of the foot was determined using the average distance between the ankle and the middle of the shoe-size-matched targets of the calibration trials.
				Normalized walking speed	%	Walking speed divided by walking speed of the 8MWT times 100%.
Narrow walkway	2	WW = 1.5*SW + FW $WW = SW + FW$	Walking between the lines of the walkway.	Success rate	%	Number of steps inside the walkway divided by the total number of steps taken times 100%.
				Normalized walking speed Normalized step width	%	Walking speed divided by walking speed of the 8MWT times 100%. Step width divided by the imposed step width times 100%.

Tasks		# Trials	Level of difficulty	Characteristics	Outcome measure	Unit	Calculation
Speed adjustments	SU SD	2 2	120% SSWS 140% SSWS 80% SSWS 60% SSWS	Start walking and when a speed cue appears one meter in front of the subjects it has to be followed at the imposed speed.	Success rate	%	The percentage of the time spend walking faster (or slower) than the imposed speed minus (or plus) 20% during the period in which the speed cue was visible. Walking speed divided by the imposed
Slalom		2	Symmetric distance between obstacles Variable distance	Walking around the moving obstacles that approach the	walking speed Success rate	%	walking speed times 100%. Number of successfully avoided obstacles divided by the number of obstacles presented times 100%.
			between obstacles	subjects with a speed of 50% SSWS.	Normalized walking speed	%	Walking speed divided by walking speed of the 8MWT times 100%.
Turning	HT	2	$ \begin{array}{l} ART = 3s \\ ART = 2s \end{array} $	Start walking and when a turning cue approaches the	Success rate	%	Number of successful half turns divided by the number of half turns times 100%.
				subject with a speed of 100% SSWS, the subject has to turn and walk back to the start.	Turning time	S	Time within the turning square (for full turns) or time from appearance of the turning cue till moment walking direction was reversed (for half turns), using the data of the spine shoulder.
	FT	1		In the two presented squares the subject has to make a full turn as fast and safe as possible in the direction of the arrow			
Dual-task walking	PDT	2		Walking while also performing a dual	Normalized walking speed	%	Walking speed divided by walking speed of the 8MWT times 100%.
				task. The dual task was an auditory Stroop task.	Success rate dual task	%	Number of correct responses divided by the number of stimuli given times 100%.
	ADT	5	ART = 1 s (three trials) ART = 0.75 s (two trials)	Avoiding suddenly appearing obstacles while also performing a dual task. The dual task was an auditory	Normalized success rate	%	Obstacle avoidance success rate divided by success rate of the obstacle avoidance task times 100%, excluding subjects that had an obstacle-avoidance success rate of 0% at baseline.
				Stroop task.	Success rate dual task	%	Number of correct responses divided by the number of stimuli given times 100%, excluding subjects that had an obstacle-avoidance success rate of 0% at baseline.
Total		35					

SSS: symmetric stepping stones; ISS: irregular stepping stones; SU: speeding up; SD: slowing down; HT: half turns; FT: full turns; PDT: plain dual-task walking (8meter walking test with dual task); ADT: augmented dual-task walking (obstacle avoidance with dual task); ART: available response time; SL: step length; WW: walkway width; SW: step width; FW: foot width; SSWS: self-selected walking speed of unconstrained walking.

speed during the 8-m walking test and available response distance (Figure 2). Subsequently, the 8-m walking test was performed with the dual task (i.e., plain dual-task walking), preceded by a familiarization trial in which the auditory Stroop task was practiced while sitting. The remaining Interactive Walkway tasks were randomized in blocks (Table 2), with difficulty level randomized within the blocks and sufficient rest breaks in between trials to prevent fatigue. Stroke patients were permitted to use walking aids, including quad canes (n = 3), canes (n = 4), ankle foot orthoses (n = 11) and functional electrical stimulation (n = 1).

Data pre-processing and analysis

Data pre-processing followed Geerse et al. [11,12], as detailed in Supplementary file S1. The outcome measures of the Interactive Walkway tasks were calculated from specific body points' time series (i.e., 3D time series of the ankles, spine base and spine shoulder), estimates of foot contact and foot off and step locations, as detailed in Table 2 and Supplementary file S1. The average over trials per task per subject was calculated for all outcome measures.

Statistical analysis

The known-groups validity of clinical test scores, spatiotemporal gait parameters and Interactive Walkway walking-adaptability outcome measures was evaluated by comparing them between stroke patients and controls using independent-samples *t*-tests. We computed r ($r = \sqrt{t^2/(t^2 + df)}$) to quantify the effect sizes, where values between 0.100 and 0.299 were regarded as small, between 0.300 and 0.499 as medium and above 0.500 as large effect sizes [24].

Pearson's correlation coefficients were determined only for stroke patients and calculated between Interactive Walkway walking-adaptability outcome measures and commonly used clinical test scores of walking ability and spatiotemporal gait parameters of unconstrained walking. Absolute correlations between 0–0.499, 0.500–0.699, 0.700–0.899 and 0.900–1.000 were regarded as low, moderate, high and very high, respectively [25]. SPSS version 24 (IBM[©] SPSS[©], Armonk, New York, United States) was used to perform the statistical analyses. Alpha was set at 0.05. No adjustment for multiple comparisons was made due to the exploratory nature of this study.

Results

In total, 30 stroke patients and 30 age- and sex-matched controls (mean ± std: 62.5 ± 10.1 vs. 62.9 ± 10.3 years, respectively; 18 males and 12 females in each groups) were included in this study. Stroke patients were 7.9 ± 7.3 years post-stroke, had a Fugl-Meyer Assessment lower extremity score of 19.7 ± 7.4 (possible range 0–34; higher scores indicate better motor function) and a Montreal Cognitive Assessment score of 24.9 ± 2.9 (possible range 0–30; higher scores indicate better cognitive abilities), which was not assessed in five stroke patients due to (severe) aphasia. Controls had a significantly higher Montreal Cognitive Assessment score of 27.7 ± 1.4 (p < 0.001).

In total, 91 trials (4.2% of all trials; 5.0–13.3% of trials per task) were not performed (63 trials; four patients were unable to complete all trials due to a reduced fitness level) or were not recorded correctly (28 trials; due to experimentation errors or one or more Kinect sensors failing to recognize stroke or control subjects).

Known-groups validity

Stroke patients performed significantly worse on all clinical tests compared to controls ($p \le 0.001$; Table 3). This was also seen for the spatiotemporal gait parameters: all outcome measures showed values associated with lower walking speeds, wider step widths and less symmetric steps for stroke patients (p < 0.001; Table 3). Furthermore, stroke patients performed significantly worse than controls on all Interactive Walkway walking-adaptability outcome measures, except stepping accuracy on irregular stepping stones, normalized walking speed of speeding up trials,

Table 3. Means, standard deviations and between-groups statistics of outcome measures of clinical tests, unconstrained walking and walking adaptability tasks on the Interactive Walkway for stroke patients and controls.

			Stroke mean + std	Control mean + std	t-value	n-value	r-value
Clinical tests			incur ± sta	incur ± sta	t value	<i>p</i> vulue	7 70100
Timed-Up-and-Go test	Time (s)*		17.3 + 11.4	7.4 + 2.2	$t_{21.1} = -4.62$	< 0.001	0.638
10-m walking test	Time (s)*	CWS	16.6 + 13.2	7.3 ± 1.0	$t_{20,2} = -3.83$	0.001	0.577
to the training test	Time (s)*	MWS	13.5 ± 11.3	5.3 ± 0.8	$t_{29.3} = -3.94$	< 0.001	0.588
Tinetti Balance Assessment	Score*		21.1 ± 5.0	27.7 ± 0.5	$t_{29.5} = 7.19$	< 0.001	0.797
7-item Berg Balance Scale	Score*		10.0 ± 2.5	13.3 ± 1.3	$t_{42.8} = 6.50$	< 0.001	0.701
Functional Reach Test	Reaching distance (cm)*		22.3 ± 7.2	29.9 ± 5.6	$t_{58} = 4.60$	<0.001	0.517
Unconstrained walking							
8-m walking test	Walking speed (cm/s)*		83.0 ± 34.6	134.3 ± 19.0	$t_{45.0} = 7.11$	< 0.001	0.727
2	Step length (cm)*		52.4 ± 14.2	74.5 ± 9.4	$t_{50.3} = 7.10$	< 0.001	0.707
	Stride length (cm)*		105.3 ± 28.7	149.9 ± 18.7	$t_{49.8} = 7.13$	< 0.001	0.711
	Step width (cm)*		17.3 ± 5.5	11.1 ± 2.8	$t_{43,3} = -5.55$	< 0.001	0.645
	Cadence (steps/min)*		94.0 ± 20.5	112.3 ± 7.5	$t_{36.7} = 4.57$	< 0.001	0.602
	Step time (s)*		0.669 ± 0.184	0.526 ± 0.038	$t_{31.4} = -4.15$	< 0.001	0.595
	Stride time (s)*		1.335 ± 0.378	1.047 ± 0.074	$t_{312} = -4.10$	< 0.001	0.591
	Symmetry step length (%)*		85.5 ± 15.0	96.6 ± 2.3	$t_{30.3} = 4.03$	< 0.001	0.591
	Symmetry step time (%)*		78.7 ± 13.8	96.1 ± 2.9	$t_{31.5} = 6.80$	<0.001	0.771
Walking adaptability							
Obstacle avoidance	Margins trailing limb (cm)*		9.0 ± 8.4	19.9 ± 7.3	$t_{58} = 5.38$	< 0.001	0.577
	Margins leading limb (cm)*		2.3 ± 6.8	12.1 ± 6.1	$t_{58} = 5.88$	< 0.001	0.611
	Success rate (%)*		45.1 ± 32.4	88.2 ± 11.3	$t_{35.9} = 6.88$	< 0.001	0.754
Sudden stops-and-starts	Sudden-stop margins (cm)*		-1.8 ± 7.2	5.4 ± 9.2	$t_{57} = 3.33$	0.002	0.403
	Success rate (%)*		56.5 ± 25.9	76.8 ± 18.5	$t_{50.7} = 3.46$	0.001	0.437
	Initiation time $(s)^*$		1.653 ± 0.462	1.338 ± 0.235	$t_{41.3} = -3.28$	0.002	0.455
Goal-directed stepping	Stepping accuracy (cm)*	SSS	3.7 ± 1.7	2.5 ± 0.7	$t_{35.6} = -3.48$	0.001	0.504
	Normalized walking speed (%)*	SSS	78.5 ± 18.9	96.0 ± 16.5	$t_{56} = 3.77$	<0.001	0.449
	Stepping accuracy (cm)	ISS	4.8 ± 2.1	3.9 ± 1.0	$t_{40.4} = -1.97$	0.056	0.296
	Normalized walking speed (%)*	ISS	77.7 ± 18.4	96.0 ± 15.7	$t_{57} = 4.11$	<0.001	0.478
Narrow walkway	Success rate (%)*		68.7 ± 27.4	84.3 ± 17.4	$t_{57} = 2.62$	0.011	0.328
	Normalized walking speed (%)*		80.4 ± 17.3	99.0 ± 11.9	$t_{57} = 4.83$	<0.001	0.539
	Normalized step width (%)*		66.8 ± 30.2	37.7 ± 16.1	$t_{57} = -4.64$	<0.001	0.523
Speed adjustments	Success rate (%)*	SU	58.5 ± 13.9	69.7 ± 10.1	$t_{47.0} = 3.46$	0.001	0.450
	Normalized walking speed (%)	SU	87.8 ± 9.9	90.2 ± 6.7	$t_{44.8} = 1.07$	0.291	0.158
	Success rate (%)*	SD	72.3 ± 6.8	79.1 ± 5.2	$t_{55} = 4.24$	<0.001	0.496
	Normalized walking speed (%)*	SD	102.9 ± 4.1	99.4 ± 2.3	$t_{40.1} = -3.94$	<0.001	0.528
Slalom	Success rate (%)*		43.3 ± 21.1	55.3 ± 23.0	$t_{54} = 2.03$	0.048	0.266
	Normalized walking speed (%)*		79.8 ± 15.5	94.7 ± 9.6	$t_{40.5} = 4.23$	< 0.001	0.554
Turning	Success rate (%)*	HT	11.1 ± 25.3	65.0 ± 35.1	$t_{52.6} = 6.69$	< 0.001	0.678
	Turning time (s)	HT	1.533 ± 0.285	1.435 ± 0.251	$t_{55} = -1.38$	0.174	0.182
	Iurning time (s)*	FT	$6.1 64 \pm 4.508$	2.149 ± 0.961	$t_{28.1} = -4.53$	< 0.001	0.650
Dual-task walking	Normalized walking speed (%)*		79.7 ± 14.2	8/./±9.5	$t_{56} = 2.54$	0.014	0.321
	Success rate dual task (%)*	PDI	//.4±21.6	94.9 ± 12.2	$t_{43.9} = 3.80$	< 0.001	0.498
	Normalized success rate (%)	ADI	80.8 ± 69.3	97.2 ± 23.9	$t_{27.4} = 1.11$	0.2/7	0.208
	Success rate dual task (%)*	ADT	68.3 ± 24.8	91.6 ± 9.2	$t_{28.1} = 4.38$	<0.001	0.637

CWS: comfortable walking speed; MWS: maximum walking speed; SSS: symmetric stepping stones; ISS: irregular stepping stones; SU: speeding up; SD: slowing down; HT: half turns; FT: full turns; PDT: plain dual-task walking (8-meter walking test with dual task); ADT: augmented dual-task walking (obstacle avoidance with dual task).

*Significant between-groups difference (p < 0.05).



Figure 3. Overview of the correlation coefficients between commonly used clinical test scores [TUG, 10MWT-CWS, 10MWT-MWS, TBA, BBS, FRT] (*x*-axis), spatiotemporal gait parameters of unconstrained walking [UW1-9] (*x*-axis) and Interactive Walkway walking-adaptability outcome measures (OA1-3, SSS1-3, GDS1-4, NWW1-3, SA1-4, S1-2, T1-3, DT1-4; *y*-axis) in stroke patients. The order and abbreviations of the outcome measures on the axes is in agreement with Table 3.

turning time of half turns and normalized success rate during augmented dual-task walking (Table 3).

Correlations

For the vast majority of walking-adaptability outcome measures we found no-to-moderate correlations with clinical test scores and unconstrained-walking parameters. That is, of the 156 possible correlations between clinical test scores and Interactive Walkway walking-adaptability outcome measures (left block in Figure 3), 56 (35.9%) were significant, out of which 2 (1.3%) were very high, 4 (2.6%) were high, 31 (19.9%) were moderate and 19 (12.2%) were low. Of the 234 possible correlations between spatiotemporal gait parameters of unconstrained walking and Interactive Walkway walking-adaptability outcome measures (right block in Figure 3), 70 (29.9%) were significant, out of which 15 (6.4%) were high, 32 (13.7%) were moderate and 23 (9.8%) were low.

Discussion

A stroke may result in impaired walking adaptability, affecting the ability to negotiate environmental challenges, which potentially contributes to the high fall risk seen in this population [8]. Assessments of walking adaptability may guide gait rehabilitation programs or contribute to the design of future targeted and individualized interventions directed at improving safe community ambulation after stroke. However, currently available assessments of walking ability after stroke hardly take walking adaptability into account [1]. We therefore evaluated the potential of the Interactive Walkway as a new technology for a quick, unobtrusive and comprehensive quantitative assessment of walking adaptability inty in stroke patients.

As a first step, we evaluated its known-groups validity. As expected, for almost all outcome measures stroke patients performed significantly worse than controls (Table 3). Group differences for spatiotemporal gait parameters of unconstrained walking, as measured with the Interactive Walkway, were as expected [26-28] and in line with the results of an earlier study showing that the Kinect v2 sensor can measure spatiotemporal gait parameters with considerable accuracy in stroke patients [29]. Also in accordance with the findings of previous studies, Interactive Walkway outcome measures of the various walkingadaptability tasks revealed that stroke patients have problems avoiding obstacles [2,4,5], making sudden step adjustments [30,31], making full turns [32] and combining walking with secondary tasks [9,28]. Besides, normalized walking speeds were significantly lower for stroke patients, indicating that they adjusted their walking speed more than controls when walking in complex environments. These results emphasize the importance of assessing walking adaptability in an overground setting, which allows stroke patients to lower their walking speed depending on their ability to meet environmental demands [10]. In the current study, only stepping accuracy of the irregular stepping stones, normalized walking speed of speeding up trials, turning time of half turns and normalized success rate of augmented dual-task walking did not exhibit significant group differences. Nonetheless, medium and large effect sizes were found for all other Interactive Walkway outcome measures with differences occurring in the expected direction. Therefore, the results of this study suggest good known-groups validity for Interactive Walkway walkingadaptability tasks, similar to that of clinical tests of walking ability and spatiotemporal gait parameters quantified for unconstrained walking.

We assessed walking adaptability guite broadly and found that not all of the assessed tasks need to be included for a comprehensive assessment of walking adaptability. That is, Interactive Walkway tasks whose outcome measures do not exhibit group differences or are highly correlated with commonly used clinical test scores and/or uncontrained walking parameters can be excluded because they add little information. In this study, this concerned sudden starts, speed adjustments, full turns and augmented dual-task walking tasks. The vast majority of Interactive Walkway walking-adaptability tasks appeared to complement clinical test scores and unconstrained walking parameters, as evidenced by no-to-moderate correlations (Figure 3). The various walking-adaptability tasks also seemed to assess different aspects of walking adaptability. That is, correlations among outcomes of the various walking-adaptability tasks were generally not significant (see Supplementary file S2), in contrast to clinical test scores and spatiotemporal gait parameters, which were highly interrelated and hence often somewhat redundant with one another. A comprehensive assessment of walking adaptability should thus include multiple complementary and discriminative Interactive Walkway tasks, such as obstacle avoidance, goal-directed stepping, narrow walkway and plain dual-task walking. A benefit of assessing walking adaptability comprehensively is that it may reveal specific walking limitations, which could then be targeted in individualized training programs [33,34]. Van Swigchem et al. [4] found that even in mildly affected stroke patients walking adaptability may be reduced, possibly increasing their risk of falling. Training of walking adaptability, overground or on a treadmill, has shown to be effective in improving walking ability in stroke patients [3,8,35,36] and in reducing risk of falling [8]. Interactive Walkway walking-adaptability assessments may assist in optimizing and patient-tailoring gait training programs by adjusting the training content and difficulty level to the specific needs and competences of the patient.

With this study, we examined the potential of walking-adaptability tasks on the Interactive Walkway for discriminating between stroke patient and controls and for providing information complementary to clinical test scores of walking ability and unconstrained walking parameters. Recent work found that walking-adaptability tasks also provide relevant information for the identification of fallers [37]. Poor performance on the obstacleavoidance and goal-directed stepping tasks were identified as risk factors for future falls [37]. Identifying such walking-related fallrisk factors, which is possible with the Interactive Walkway, may further lead to more targeted, personalized and possibly more effective falls-prevention interventions.

One of the limitations of this study was that clinical tests, unconstrained walking and walking adaptability were only assessed in a single session. Future studies should examine their test-retest reliability to estimate minimal detectable change scores and responsiveness of the outcome measures that are essential for monitoring progress in gait rehabilitation. This can be done for a subset of tasks, namely those tasks that are deemed discriminative and complementary (as determined in the current study and in a recent related study with Parkinson's disease patients [38]) as well as tasks yielding potential risk factors for falls [37]. A second limitation is that we noticed that the available response times were significantly lower for stroke patients on some walking-adaptability tasks, which were caused by a higher self-selected walking speed in those tasks than in the preceding unconstrained walking task. This could have negatively influenced the outcome measures on these tasks and as such have amplified group differences. In future studies the available response times should preferably be based on a real-time indication of walking speed, which is guite feasible with the Interactive Walkway. A third limitation could be that the Interactive Walkway only uses 2D projections to evoke step responses, which do not actually pose a physical risk for the patient. Although walking-adaptability tasks with 2D projections appeared effective, given the observed group differences with overall medium to large effect sizes, it may differ from interacting with real context. For example, Timmermans et al. [10] recently observed that task prioritization differed in stroke patients negotiating physical and projected obstacles while concurrently performing an attention-demanding cognitive task: obstacle-avoidance performance was prioritized with physical obstacles, cognitive-task performance was prioritized with projected obstacles [10].

Conclusion

We conclude that Interactive Walkway walking-adaptability assessments have good known-groups validity and provide information that is complementary to clinical test scores of walking ability and unconstrained walking parameters in stroke patients.

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Data availability statement

The data that support the findings of this study are available from the corresponding author, DJG, upon reasonable request.

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