

1 Learning Effects in Psychophysical Tests of Spectral and
2 Temporal Resolution.

3
4 Monique A. M. de Jong, MD¹, Jeroen J. Briaire, PhD¹, and prof. Johan H.M.
5 Frijns, MD, PhD¹²

6 ¹ ENT Department, Leiden University Medical Centre, Leiden, The Netherlands

7 ² Leiden Institute for Brain and Cognition, Leiden University, Leiden, The
8 Netherlands

9
10 Financial Disclosures/Conflicts of Interest: This research was supported by non-
11 restrictive research funding from Advanced Bionics.

12
13 Corresponding author: Johan H.M. Frijns, ENT Department, Leiden

14 University Medical Centre

15 PO Box 9600

16 2300 RC Leiden, The Netherlands

17 Email: J.H.M.Frijns@lumc.nl

18 Telephone number: +31 (0)71 52 611 79

19

20 **Abstract**

21

22 **Objectives:** Psychophysical tests of spectral and temporal resolution, such as the
23 spectral-ripple discrimination task and the temporal modulation detection test,
24 are valuable tools for evaluation of cochlear implant performance. Both tests
25 correlate with speech intelligibility and are reported to show no instantaneous
26 learning effect. However, some of our previous trials have suggested there is a
27 learning effect over time. The aim of this study was to investigate the test-retest
28 reliability of the 2 tests when measured over time.

29 **Design:** Ten adult cochlear implant recipients, experienced with the
30 HiResolution speech coding strategy, participated in this study. Spectral ripple
31 discrimination and temporal modulation detection ability with the HiResolution
32 strategy were assessed both before and after participation in a previous trial that
33 evaluated 2 research speech coding strategies after 2 weeks of home-usage. Each
34 test was repeated six times on each test day.

35 **Results:** No improvement was observed for same-day testing. However,
36 comparison of the mean spectral ripple discrimination scores before and after
37 participation in the take-home trial showed improvement from 3.4 to 4.8 ripples
38 per octave ($p < 0.001$). The mean temporal modulation detection thresholds
39 improved from -15.2 dB to -17.4 dB ($p = 0.035$).

40 **Conclusions:** There was a clear learning effect over time in the spectral and
41 temporal resolution tasks, but not during same-day testing. Learning effects may
42 stem from perceptual learning, task learning or a combination of those two
43 factors. These results highlight the importance of a proper research design for
44 evaluation of novel speech coding strategies, where the baseline measurement is

45 repeated at the end of the trial to avoid false positive results as a consequence of
46 learning effects.

47

49 Psychophysical tests of spectral and temporal resolution, such as the spectral-
50 ripple test (Won et al. 2007; Drennan et al. 2010; Won et al. 2010; Anderson et al.
51 2012; Aronoff & Landsberger 2013; Jones et al. 2013) and the temporal
52 modulation detection test, (Shannon 1992; Won et al. 2011; Fraser & McKay
53 2012) are valuable tools for the evaluation of cochlear implant (CI) hearing
54 during clinical trials. The extent to which the implementation of novel
55 technologies affects the performance of CI recipients is often too mild to detect
56 with traditional speech or music outcome measures. Psychophysical measures
57 are more sensitive to processor changes as they allow for the evaluation of basic
58 abilities, such as spectral and temporal resolution (Buechner et al. 2008; Brendel
59 et al. 2008; Drennan et al. 2010), which are fundamental aspects of how well
60 people hear. Both tests have been shown to correlate independently with vowel,
61 consonant, and speech recognition in CI recipients (Fu 2002; Henry et al. 2005;
62 Won et al. 2007; Won et al. 2013; Holden et al. 2016; Zhou 2017).

63 It is generally assumed that the evaluation of basic psychophysical
64 capabilities yields a measure of hearing that does not change over time (Won et
65 al. 2007; Drennan et al. 2010). Previous studies have investigated potential ‘task
66 learning effects’ of spectral and temporal measurements, that is, improvement in
67 performance caused by practice with the task rather than actual improvement in
68 spectral and/or temporal resolution. No task learning effect was found in an acute
69 setting, when tasks were repeated up to nine times (Won et al. 2007; Drennan et
70 al. 2008; Drennan et al. 2010). To the best of our knowledge, only 1 study
71 examined the test-retest reliability of the spectral-ripple threshold measurement
72 over a longer period of time in experienced CI users (Won et al. 2007). No task

73 learning effect was found when repeating the task on separate test days,
74 although, no time interval between the measurements was reported. Drennan et
75 al. (2015) studied learning in both spectral and temporal modulation tests in
76 newly implanted CI users and, on average, did not find a significant
77 improvement over the first 12 months after activation. However, 20% of the
78 individuals significantly improved on both tasks and another 20% significantly
79 deteriorated.

80 The previously mentioned studies suggest that spectral and temporal
81 testing serve as useful, and most probably also reliable diagnostic tools for
82 assessment of CI outcome in a research setting. However, we have observed
83 somewhat different outcomes in our research center. The modified spectral ripple
84 test (SMRT), developed by Aronoff & Landsberger (2013), and the modulation
85 detection threshold (MDT) test, adapted from Bacon & Viemeister (1985), are
86 frequently used in the evaluation of novel processing strategies in the Leiden
87 University Medical Center (LUMC), the Netherlands. As a limited number of CI
88 users are available for research purposes, many of our subjects have participated
89 in multiple studies over the last few years. As a result, these subjects have had
90 substantial practice on the SMRT and MDT test with several different speech
91 coding strategies. We noticed higher SMRT and MDT scores in these more
92 practiced CI users and therefore hypothesize that the psychophysical
93 performance among these CI recipients improved because of this practice.

94 It is well known that CI recipients improve performance in the first few
95 months after implantation (Staller et al. 1997; Rouger et al. 2007; Ruffin et al.
96 2007). It is plausible that this improvement is caused by ‘perceptual learning’,
97 which is a process by which the ability of the auditory system to process stimuli

98 is improved through experience. Also Moberly et al. (2015) suggested that CI
99 users could learn from new speech cues, which might be present in novel speech
100 coding strategies. Repeated testing with the SMRT and MDT test in a research
101 setting with multiple novel speech coding strategies could, therefore, lead to both
102 task and perceptual learning and consequently to improved SMRT and MDT
103 performance. The present study assessed performance on the SMRT and MDT
104 test before and after participation in a previous take-home trial, in which 2
105 experimental speech coding strategies were evaluated.

106 MATERIALS AND METHODS

107 Subjects

108 A group of 10 adult cochlear implant (CI) recipients who had been implanted
109 with a HiRes90K device with HiFocus 1J or a CII device with HiFocus with a
110 positioner electrode array (Advanced Bionics, Sylmar, CA) at the LUMC were
111 recruited for this study. All had used the Harmony processor programmed with
112 the HiResolution (HiRes) speech coding strategy for multiple years. Subject
113 demographics are shown in Table 1. Ages ranged from 43 to 74 years with a
114 mean of 60.2 years. The average duration of deafness was 26.6 years (range 4-67
115 years) and average implant experience was 98 months (range 31-174 months).
116 Mean phoneme scores on open set Dutch monosyllabic consonant-vowel-
117 consonant (CVC) words in quiet conditions at 65 dB were 89.3% (range 76-96%).

118 Protocol and speech coding strategies

119 Spectral ripple discrimination and temporal modulation transfer functions were
120 assessed at baseline (week 0) and 2, 4, and 6 weeks after the baseline measures.
121 Participants were tested twice (at t=0 weeks and t=6 weeks) with their standard

122 clinical speech coding strategy, HiRes. This is a bandpass filter based strategy
123 that uses a traditional processing approach in which channel-specific temporal
124 envelopes are extracted and delivered with interleaved, high-rate pulse trains.
125 More detailed information about this speech coding strategy is provided by Firszt
126 (2003).

127 The examinations at week 2 and 4 were part of a separate take-home trial, in
128 which 2 variations of the HiRes speech coding strategy, which applied different
129 filtering techniques, were evaluated. The 2 experimental strategies, HiRes FFT
130 and HiRes Optima (Advanced Bionics, reference note 1), utilize a finite impulse
131 response filter in conjunction with Fast Fourier Transformation (FFT)
132 processing. HiRes Optima also uses current steering to create up to 135 virtual
133 spectral channels. In fact, it is a more energy-efficient variation of HiRes Fidelity
134 120 (Firszt et al. 2009). As the number of excitable channels is increased with
135 HiRes Optima, an improved performance on the SMRT is expected as compared
136 to both HiRes and HiRes FFT, as was demonstrated for HiRes Fidelity 120 by
137 Drennan et al. (2010). However, these authors also argued that FFT processing
138 potentially decreases temporal resolution, due to spectral smearing. Therefore,
139 both HiRes FFT and HiRes Optima might decrease performance on the MDT
140 test. To eliminate order and practice effects, the participants received the 2
141 experimental take-home strategies in randomized order and had the chance to
142 adapt to the strategies during the 2 weeks prior to the testing. In this paper, the
143 randomization allows for the evaluation of test date effects (between week 2 and
144 4) while minimizing the effects of processing strategy. In other words, in the
145 paired comparison between performance at week 2 and 4, half of the participants
146 was using HiRes FFT and half was using HiRes Optima at each test session.

147 Because the order of strategy was randomized, the effect of strategy was
148 minimal. The current study was approved by the Medical Ethical Committee of
149 the LUMC (ref. P02.106.Y).

150 **Psychophysical testing:**

151 During all psychophysical tasks, the listeners were seated in a double-walled
152 sound-attenuating booth. Sounds were presented via a single loudspeaker, placed
153 1 meter from the listener at 0 degrees and level with the listener's head. Subjects
154 received instructions for the psychophysical tests and then practiced the tasks six
155 times or more if necessary, to avoid learning in the actual test setting. Listeners
156 responded using a mouse with a custom computer interface, or they responded
157 verbally when they were unable to use the mouse (for example subject 10 was
158 visually impaired). All stimuli were presented at 65 dB (SPL).

159 Spectral resolution was examined with the spectral-temporally modulated
160 ripple test (SMRT) as developed by Aronoff & Landsberger (2013). In this
161 adaptive 3-alternative forced choice task, listeners were asked to discriminate a
162 spectrally rippled stimulus, that is, a stimulus that is amplitude modulated in
163 the frequency domain, from a reference stimulus. The reference stimuli had fixed
164 ripple densities of 20 ripples per octave (RPO), whereas the ripple density of the
165 target stimulus was modified until the listener was unable to discriminate
166 between the stimuli. The SMRT differs from previous spectral ripple tests (e.g.
167 Henry & Turner 2003) in that the ripple stimuli are modified. The SMRT uses a
168 spectral ripple with a modulation phase that drifts with time (See fig. 1a in
169 Aronoff & Landsberger 2013), thereby avoiding loudness cues and edge effects.
170 No feedback about the correct answer was given. The procedure was repeated six

171 times per testing run, and the estimated thresholds were averaged as the final
172 SMRT score.

173 The temporal modulation transfer function (TMTF) test, a 2-alternative
174 forced choice measure of temporal resolution, was used to determine the
175 modulation depth detection threshold (MDT) (Won et al. 2011). Two 1-second
176 intervals consisting of wide band noise were presented to the listener. While the
177 reference stimulus was unmodulated, the target stimulus was amplitude
178 modulated in the time domain with a frequency of 100 Hz and a starting
179 modulation depth of 100%, because these conditions, when combined with
180 spectral ripple thresholds, accounted for the highest amount of speech variance
181 in previous studies (Won et al. 2011). Subjects were instructed to choose the
182 interval that contained the modulated noise after which feedback of the correct
183 answer was provided. A 2-down, 1-up adaptive procedure was used to obtain
184 MDTs in dB relative to 100% modulation [$20\log_{10}(\text{modulation depth})$]. The
185 average of six tracking histories provided the final MDT score.

186 **Statistical analysis**

187 A 2-way repeated measures analysis of variance (ANOVA) using within-subject
188 factors of ‘visit’ (Week numbers) and ‘repetition number’ (Repetition number 1-6)
189 were used to determine if there was a main effect of visit, repetition number, and
190 an interaction between those two factors. Because two different strategies were
191 examined in randomized order in week 2 and 4, those weeks could not be
192 compared to week 0 or 6. Therefore, only week 0 and 6 were compared to each
193 other and week 2 was compared to week 4. SPSS Statistics Version 20 was used
194 for calculations.

RESULTS

195
196 Individual and mean SMRT scores per test day are demonstrated in Figures 1A
197 and 1B. The average scores of the six repetitions was 3.4 RPO at baseline and 4.2
198 RPO, 5.0 RPO, and 4.8 RPO at weeks 2, 4, and 6, respectively. The results from a
199 2-way repeated-measures ANOVA indicated a highly significant improvement
200 between baseline and 6-week SMRT thresholds ($F_{1,9}=52.2$, $p<0.001$), which was
201 present for all ten subjects (Fig.1). No significant effect of repetition number
202 ($F_{5,45}=1.5$, $p=0.195$) or interaction between visit and repetition number
203 ($F_{5,45}=1.398$, $p=0.243$) was observed. There was no significant difference
204 between SMRT scores at week 2 and 4 ($F_{1,9}=1.755$, $p=0.218$) (Fig. 1B). Figure 2
205 shows the individual and mean SMRT thresholds as a function of trial number at
206 instantaneous testing, i.e. repeating the task on the same test day. A 2-way
207 repeated-measures ANOVA using the Greenhouse-Geisser correction revealed no
208 learning over the course of the six repeated runs on a given test day when all 4
209 test days were included ($F_{2.4,21.5}=2.347$, $p=0.112$). When comparing the first
210 with the last measurements in the sequence of six, a borderline significant
211 improvement of 0.7 RPO was found ($F_{1,9}=5.012$, $p=0.052$).

212 Individual and mean MDT scores are shown in Figures 3A and 3B. The mean
213 MDT scores at weeks 0, 2, 4, and 6 were -15.2 dB, -16.5 dB, -17.2 dB, and -17.4
214 dB, respectively, relative to 100% amplitude modulation. A 2-way repeated-
215 measures ANOVA showed that there was a significant improvement between the
216 first and second six repetitions with the HiRes speech coding strategy, i.e. week 0
217 versus week 6 ($F_{1,9}=6.108$, $p=0.035$) (Fig. 3A). No effect of repetition number
218 ($F_{5,45}=0.965$, $p=0.449$) or interaction between visit and repetition number

219 (F5,45=0.483, p=0.787) was observed. As 1 outlier was observed in this analysis
220 (subject 1), the repeated-measures ANOVA was repeated while excluding the
221 outlier, resulting in mean scores of -16.1 dB at baseline and -17.4 at 6 weeks. The
222 improvement appeared to still be highly statistically significant (F1,8=23.7,
223 p=0.001), and still revealed no effect of repetition number (F5,40=1.018, p=0.420)
224 or interaction between visit and repetition number (F5,40=0.709, p=0.620). The
225 MDT scores at weeks 2 and 4 were not significantly different from each other
226 (F1,9=0.608, p=0.456) (Fig. 3B) and a 2-way repeated-measures ANOVA using
227 the Greenhouse-Geisser correction to adjust for non-sphericity revealed no effect
228 of repetition number when all 4 test days were included (F2.2, 19.9=0.967,
229 p=0.405). Moreover, no improvement was observed between the first and last of
230 the six repetitions (F1,9=2.289, p=0.165). Altogether, these findings indicated no
231 instantaneous learning effect (Fig. 4). A Pearson product-moment correlation
232 coefficient was computed to assess the relationship between the SMRT and MDT
233 scores, and revealed a significant correlation between the two measures,
234 $R^2=0.298$, $p<0.001$.

235

236

DISCUSSION

237 The present study demonstrated a clear significant learning effect over time for
238 both the SMRT and the MDT test after repeated examination with the use of
239 different speech coding strategies. Group spectral-ripple discrimination ability
240 improved from 3.4 RPO at baseline to 4.8 RPO at the retest measurement after
241 participation in a clinical trial. The difference was significant on the individual
242 level in five out of ten subjects. The MDT results improved from -15.2 dB to -17.4

243 dB, a difference of -2.2 dB group-wide in the same time interval. Two out of ten
244 individual participants improved significantly. None of the listeners deteriorated
245 in performance and, in line with previous literature (Won et al. 2007; Drennan et
246 al. 2008; Drennan et al. 2010), no learning was observed for either task in an
247 acute setting.

248 Although no instantaneous learning effect was detected in this or previous
249 studies, there are also studies that conclude that there is no learning over time.
250 However, this previous research on learning effects mainly focused on acute
251 settings, and if long-term learning was assessed, either the duration was poorly
252 reported or learning effects after longer time intervals (at least 2 months) were
253 investigated (Won et al. 2007; Drennan et al. 2014; Drennan et al. 2015). During
254 clinical take-home trials, when the presence of a potential learning effect is
255 essential for the interpretation of results, participants are typically exposed to
256 multiple speech coding strategies and execute the psychophysical tasks relatively
257 frequently, e.g., every 2-4 weeks. This makes it essential to identify learning
258 effects in these time frames.

259 Multiple practice sessions with rather short time intervals introduce 2
260 potential risks; perceptual and task learning. Exposure to new speech-coding
261 strategies, and therefore novel speech cues, leads to perceptual learning. Because
262 the study population in this study participated in a clinical trial between baseline
263 and retest measurements, they did get a chance to adapt to different speech cues
264 and learn new auditory percepts. This perceptual learning could have potentially
265 been used in the spectral and/or temporal discrimination tasks (Moberly et al.
266 2015). On the other hand, speech scores were also assessed during this trial, for

267 which no improvement was observed ($F_{1,9}=0.826$, $p=0.387$). The lack of a
268 correlation between improvement of the speech scores and the SMRT or MDT
269 scores ($R=0.039$ and $R=0.073$ respectively), suggests that the potential effect of
270 perceptual learning is limited. It is reasonable to assume that repeated
271 psychophysical testing in a short period of time could cause task learning.
272 Moreover, it is well-known that perceptual learning amplifies this task learning
273 because of a so-called “carryover effect” (Liu 1999; Liu & Weinshall 2000;
274 Donaldson et al. 2011). A carryover effect is an effect, or ability, that carries over
275 from one experimental condition to another. When time intervals between test
276 sessions are sufficient, like in the study of Drennan et al. (2015), a carryover
277 effect can be considered as (at least partially) extinguished. In other words, a so-
278 called “wash-out period” of sufficient duration compensates for the carryover
279 effect. Moreover, as the purpose of Drennan et al. (2015) was to examine whether
280 basic spectral and temporal discrimination abilities would change over the first
281 year of implant use, they did not vary speech coding strategies. Hence, no
282 perceptual learning induced by the use of novel speech coding strategies could
283 occur. Given the frequency of test intervals in the current study, which was
284 comparable to many other take-home studies (e.g. Holden et al. 2013; Neben et
285 al. 2013; Frijns et al. 2013), it is possible that the duration between visits was
286 shorter than the wash-out period and therefore a carryover effect cannot be ruled
287 out. Although it is clear that a learning effect was present for both tests, the
288 current study cannot identify the exact mechanism for this effect. It could be due
289 to task learning, perceptual learning by participating in a clinical trial, or a
290 combination of both factors.

291 Our results could also partially be explained by the upward trend in
292 motivation of participants, and the placebo effect of any new speech coding
293 strategy. Moreover, the contrasting results found in this study compared with
294 previous work, could, although unlikely, be attributed to the use of different
295 versions of the psychoacoustic measures. For example, Drennan et al. (2014) used
296 a non-adaptive clinical version of the spectral ripple test, which differed
297 considerably from the spectral ripple task that was used in the current study. For
298 example, the current spectral ripple task implemented a temporal effect to avoid
299 potential loudness cues. This resulted in a significant, though fairly low,
300 correlation between SMRT and MDT scores, implying that the SMRT does not
301 purely measure spectral resolution, but is also influenced by temporal effects.
302 This emphasizes the need for an improved measure of spectral resolution, that is
303 less influenced by both loudness and temporal cues.

304 Because the order in which the two experimental strategies were examined
305 in this study was randomized, an extra analysis between the second and third
306 test day, irrespective of the speech coding strategy, could be performed. No
307 significant difference was found between the test days for either task, implying
308 that no learning, or too little effect size to reach sufficient power, is present after
309 2 blocks of testing on separate days. Unfortunately, the number of practice
310 sessions that are necessary for the learning effect to be completely extinguished
311 is unclear and information about the effect size of learning in the MDT test and
312 SMRT is not provided. In that light, it would have been helpful if basic HiRes
313 scores were evaluated at each session, regardless of what condition the subjects
314 were sent home with, although the fatigue that comes with multiple test sessions

315 on one day introduces another bias. A placebo controlled trial, in which
316 participants perform the psychophysical tasks multiple times, on separate test
317 days, with the same speech coding strategy (with a “fake” remapping in which
318 the subject may think that the strategy is different, but in fact is not), would
319 provide us with more specific information. Nevertheless, this study provides us
320 with sufficient evidence that a learning effect is present in the two tasks.

321 These results do not diminish the value of psychophysical testing for the
322 evaluation of newly developed speech coding strategies; rather, they emphasize
323 the importance of a proper, randomized research design. As a carryover effect
324 could be the cause of learning, it should be dealt with by allowing sufficient time
325 between test dates to “wash-out” the effect of the previous test. Moreover, it is
326 important to incorporate a second testing phase with the baseline speech coding
327 strategy at the end of the trial, in addition to the initial baseline measurement, if
328 one wants to conclude that one of the coding strategies under test is really
329 improving speech perception. In line with this, Donaldson et al. (2011) found a
330 significant improvement in vowel recognition the second time the baseline
331 strategy was evaluated and used these results for comparison with the research
332 strategy. Another example is the study of Vermeire et al. (2010), where an
333 experimental strategy was examined acutely and after 1, 3, 6 and 12 months of
334 usage. They found a significant improvement in speech intelligibility in noise
335 with the experimental strategy over time. However, switching back to the
336 baseline strategy resulted in a similar improvement (see fig.1. of Vermeire et al.
337 (2010)), underlining the importance of comparing speech perception results with

338 a second baseline measurement. This helps to avoid misinterpretation of
339 improvements due to learning effects as true differences between strategies.
340

341
342
343
344
345
346
347
348
349

CONCLUSIONS

The SMRT and MDT tasks show a clear learning effect over time when examined relatively frequently in a clinical trial. Although an unmistakable explanation has not been shown, these results emphasize the vigilance with which these psychophysical test should be used in clinical trials, for the explicit reason that they are assumed to not change over time. Moreover, great caution with respect to (specifically long-term) learning effects is advised for the development of new psychophysical measures.

350 **Acknowledgements**

351 We thank all our participants for their time and effort during this trial. The work
352 was financially supported by Advanced Bionics.

353 **REFERENCES**

354 Advanced Bionics (2012). HiRes™ Optima Clinical Results. *Adv. Bionics White Pap. Sylmar,*
355 *Calif.*, 1–2.

356 Anderson, E.S.E., Oxenham, A.A.J., Nelson, P.B., et al. (2012). Assessing the role of spectral
357 and intensity cues in spectral ripple detection and discrimination in cochlear-implant
358 users. *J. Acoust. Soc. Am.*, 132, 3925–3934.

359 Aronoff, J.M., Landsberger, D.M. (2013). The development of a modified spectral ripple test.
360 *J. Acoust. Soc. Am.*, 134, 217–222.

361 Bacon, S.P., Viemeister, N.F. (1985). Temporal Modulation Transfer Functions in Normal-
362 Hearing and Hearing-Impaired Listeners. *Audiology*, 24, 117–134.

363 Brendel, M., Buechner, A., Krueger, B., et al. (2008). Evaluation of the Harmony
364 soundprocessor in combination with the speech coding strategy HiRes 120. *Otol.*
365 *Neurotol.*, 29, 199–202.

366 Buechner, A., Brendel, M., Krueger, B., et al. (2008). Current steering and results from novel
367 speech coding strategies. *Otol. Neurotol.*, 29, 203–207.

368 Donaldson, G., Dawson, P., Borden, L. (2011). Within-subjects comparison of the HiRes and
369 Fidelity120 speech processing strategies: speech perception and its relation to place-
370 pitch sensitivity. *Ear Hear.*, 32, 238–250.

371 Drennan, W., Won, J., Nie, K., et al. (2010). Sensitivity of psychophysical measures to signal
372 processor modifications in cochlear implant users. *Hear. Res.*, 262, 1–8.

373 Drennan, W.R., Anderson, E.S., Won, J.H., et al. (2014). Validation of a clinical assessment of
374 spectral ripple resolution for cochlear-implant users. *Ear Hear.*, 35, 92–98.

375 Drennan, W.R., Longnion, J.K., Ruffin, C., et al. (2008). Discrimination of Schroeder-phase
376 harmonic complexes by normal-hearing and cochlear-implant listeners. *J. Assoc. Res.*
377 *Otolaryngol.*, 9, 138–149.

378 Drennan, W.R., Won, J.H., Timme, A.O., et al. (2015). Nonlinguistic Outcome Measures in
379 Adult Cochlear Implant Users Over the First Year of Implantation. *Ear Hear.*, 37, 1–11.

- 380 Firszt, J., Holden, L., Reeder, R.M., et al. (2009). Speech recognition in cochlear implant
381 recipients: comparison of standard HiRes and HiRes 120 sound processing. *Otol.*
382 *Neurotol.*, 30, 146–152.
- 383 Firszt, J.B. (2003). HiResolution™ Sound Processing. *Adv. Bionics White Pap. Sylmar, Calif.*,
384 1–4.
- 385 Fraser, M., McKay, C.M. (2012). Temporal modulation transfer functions in cochlear
386 implantees using a method that limits overall loudness cues. *Hear. Res.*, 283, 59–69.
- 387 Frijns, J.H.M., Snel-Bongers, J., Vellinga, D., et al. (2013). Restoring speech perception with
388 cochlear implants by spanning defective electrode contacts. *Acta Otolaryngol.*, 133,
389 394–9. Available at: <http://www.ncbi.nlm.nih.gov/pubmed/23294241>.
- 390 Fu, Q.-J. (2002). Temporal processing and speech recognition in cochlear implant users.
391 *Neuroreport*, 13, 1635–1639.
- 392 Henry, B., Turner, C. (2003). The resolution of complex spectral patterns by cochlear implant
393 and normal-hearing listeners. *J. Acoustical Soc. Am.*, 113, 2861–73.
- 394 Henry, B., Turner, C., Behrens, A. (2005). Spectral peak resolution and speech recognition in
395 quiet: normal hearing, hearing impaired, and cochlear implant listeners. *J. Acoustical Soc.*
396 *Am.*, 118, 1111–1121.
- 397 Holden, L., Brenner, C., Reeder, R.M., et al. (2013). Postlingual adult performance in noise
398 with HiRes 120 and ClearVoice Low, Medium, and High. *Cochlear Implant. ...*, 14, 1–22.
399 Available at:
400 <http://www.maneyonline.com/doi/abs/10.1179/1754762813Y.0000000034> [Accessed
401 November 6, 2014].
- 402 Holden, L.K., Firszt, J.B., Reeder, R.M., et al. (2016). Factors Affecting Outcomes in Cochlear
403 Implant Recipients Implanted With a Perimodiolar Electrode Array Located in Scala
404 Tympani. *Otol. Neurotol.*, 37, 1662–1668. Available at:
405 [http://content.wkhealth.com/linkback/openurl?sid=WKPTLP:landingpage&an=0012949](http://content.wkhealth.com/linkback/openurl?sid=WKPTLP:landingpage&an=00129492-201612000-00032)
406 [2-201612000-00032](http://content.wkhealth.com/linkback/openurl?sid=WKPTLP:landingpage&an=00129492-201612000-00032).
- 407 Jones, G.L., Drennan, W.R., Rubinstein, J.T. (2013). Relationship between channel interaction
408 and spectral-ripple discrimination in cochlear implant users. *J. Acoust. Soc. Am.*, 133,
409 425–433.
- 410 Liu, Z. (1999). Perceptual learning in motion discrimination that generalizes across motion
411 directions. *Proc. Natl. Acad. Sci. U. S. A.*, 96, 14085–14087.
- 412 Liu, Z., Weinshall, D. (2000). Mechanisms of generalization in perceptual learning. *Vision*
413 *Res.*, 40, 97–109.
- 414 Moberly, A.C., Bhat, J., Shahin, A.J. (2015). Acoustic Cue Weighting by Adults with Cochlear
415 Implants : A Mismatch Negativity Study. *Ear Hear.*, 37, 465–472.

- 416 Neben, N., Lenarz, T., Schuessler, M., et al. (2013). New cochlear implant research coding
417 strategy based on the MP3(000™) strategy to reintroduce the virtual channel effect.
418 *Acta Otolaryngol.*, 133, 481–90.
- 419 Rouger, J., Lagleyre, S., Fraysse, B., et al. (2007). Evidence that cochlear-implanted deaf
420 patients are better multisensory integrators. *Proc. Natl. Acad. Sci.*, 104, 7295–7300.
421 Available at: <http://www.pnas.org/cgi/doi/10.1073/pnas.0609419104>.
- 422 Ruffin, C. V., Tyler, R.S., Witt, S. a., et al. (2007). Long-Term Performance of Clarion 1.0
423 Cochlear Implant Users. *Laryngoscope*, 117, 1183–1190. Available at:
424 <http://doi.wiley.com/10.1097/MLG.0b013e318058191a>.
- 425 Shannon, R. V (1992). Temporal modulation transfer functions in patients with cochlear
426 implants. *J. Acoust. Soc. Am.*, 91, 2156–2164.
- 427 Staller, S., Menapace, C., Domico, E., et al. (1997). Speech perception abilities of adult and
428 pediatric Nucleus implant recipients using the Spectral Peak (SPEAK) coding strategy.
429 *Otolaryngol. - Head Neck Surg.*, 117, 236–242.
- 430 Vermeire, K., Punte, A.K., Van De Heyning, P. (2010). Better speech recognition in noise with
431 the fine structure processing coding strategy. *J. Oto-Rhino-Laryngology, Head Neck*
432 *Surg.*, 72, 305–311.
- 433 Won, J.H., Drennan, W.R., Kang, R.S., et al. (2010). Psychoacoustic abilities associated with
434 music perception in cochlear implant users. *Ear Hear.*, 31, 796–805.
- 435 Won, J.H., Drennan, W.R., Nie, K., et al. (2011). Acoustic temporal modulation detection and
436 speech perception in cochlear implant listeners. *J. Acoust. Soc. Am.*, 130, 376–388.
- 437 Won, J.H., Drennan, W.R., Rubinstein, J.T. (2007). Spectral-ripple resolution correlates with
438 speech reception in noise in cochlear implant users. *J. Assoc. Res. Otolaryngol.*, 8, 384–
439 392.
- 440 Won, J.H., Jones, G.L., Drennan, W.R., et al. (2013). Evidence of across-channel processing
441 for spectral-ripple discrimination in cochlear implant listeners. *J. Acoust. Soc. Am.*, 130,
442 2088–2097.
- 443 Zhou, N. (2017). Deactivating stimulation sites based on low-rate thresholds improves
444 spectral ripple and speech reception thresholds in cochlear implant users. *J. Acoust.*
445 *Soc. Am.*, 141, EL243–EL248. Available at:
446 <http://asa.scitation.org/doi/10.1121/1.4977235>.

447 **Reference notes:**

- 448 1. Advanced Bionics (2012). HiRes™ Optima Clinical Results. *Adv. Bionics*
449 *White Pap. Sylmar, Calif.*, 1–2.

450

FIGURES

451

452 Figure 1

453 A. Individual and mean spectral ripple thresholds for 10 subjects (HiRes)

454 B. The same as A, now for the HiResFFT and Optima strategies

455

456 Figure 2.

457 Effects of instantaneous learning for the spectral ripple task. The figure shows

458 individual and mean spectral ripple thresholds as a function of trial number

459 based on data from 10 subjects at 4 test intervals.

460

461 Figure 3

462 A. Individual and mean modulation detection thresholds for 10 subjects (HiRes)

463 B. The same as A, now for the HiResFFT and Optima strategies.

464

465 Figure 4.

466 Effects of instantaneous learning for the Temporal Modulation Transfer Function

467 test. The figure shows individual and mean Modulation detection thresholds as a

468 function of trial number based on data from 10 subjects at 4 test intervals.