

1 **Quantitative EEG reflects Non-Dopaminergic Disease Severity in Parkinson's Disease**

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27 **Highlights**

- 28 • EEG parameters correlate to measures of disease severity in patients with Parkinson's
29 Disease.
- 30
- 31 • Both EEG slowing and reduced connectivity correlate to non-dopaminergic disease severity.
32
- 33 • The proposed markers may be useful in the screening process for Deep Brain Stimulation.
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35

36 **Abstract**

37 **OBJECTIVE** In Parkinson's Disease (PD), measures of non-dopaminergic systems involvement may
38 reflect disease severity and therefore contribute to patient-selection for Deep Brain Stimulation
39 (DBS). There is currently no determinant for non-dopaminergic disease severity. In this exploratory
40 study, we investigated whether quantitative EEG reflects non-dopaminergic disease severity in PD.

41 **METHODS** Sixty-three consecutive PD patients screened for DBS were included (mean age $62.4 \pm$
42 7.2 years, 32% females). Relative spectral powers and the Phase-Lag-Index (PLI) reflecting functional
43 connectivity were analysed on routine EEGs. Non-dopaminergic disease severity was quantified using
44 the SENS-PD score and its subdomains; motor-severity was quantified using the MDS-UPDRS III.

45 **RESULTS** The SENS-PD composite score correlated with a spectral ratio $((\delta + \theta) / (\alpha_1 + \alpha_2 + \beta))$
46 powers) (global spectral ratio Pearson's $r=0.4$, 95% Confidence Interval (95% CI) 0.1 to 0.6), and PLI
47 in the α_2 band (10-13 Hz) ($r=-0.3$, 95%CI -0.5 to -0.1). These correlations seem driven by the
48 subdomains cognition and psychotic symptoms. MDS-UPDRS III was not significantly correlated
49 with EEG parameters.

50 **CONCLUSIONS** EEG slowing and reduced functional connectivity in the α_2 band were associated
51 with non-dopaminergic disease severity in PD.

52 **SIGNIFICANCE** The described EEG parameters may have complementary utility as determinants of
53 non-dopaminergic involvement in PD.

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56 **KEYWORDS:** 'quantitative EEG', 'Parkinson's Disease', 'Deep Brain Stimulation', 'connectivity',
57 'non-motor severity'

58 **1. Introduction**

59 Parkinson's Disease (PD) is a multisystem neurodegenerative disorder, caused by progressive
60 degeneration of both dopaminergic and non-dopaminergic neurons (Jellinger, 2012). Dopaminergic
61 neurons account primarily for the characteristic motor symptoms of PD, whilst non-dopaminergic
62 neurons account for non-motor symptoms such as impaired cognition, psychiatric manifestations or
63 sleep disturbances. PD is typically treated with oral dopaminergic medication, which alleviates motor
64 symptoms. However, medication-related motor complications occur in the majority of patients within
65 10 years of disease (Ahlskog et al. , 2001). Patients refractory to oral treatment may be eligible for
66 Deep Brain Stimulation (DBS), which ameliorates motor complications and improves quality of life
67 (Deuschl et al. , 2013). DBS is particularly effective in patients perceiving substantial motor
68 improvement of upon dopaminergic treatment (Moldovan et al. , 2015). However, non-dopaminergic
69 symptoms such as cognitive impairment,(Contarino et al. , 2007) depression (Weaver et al. , 2009),
70 speech intelligibility (Tripoliti et al. , 2011) and axial symptoms (Russmann et al. , 2004) may
71 deteriorate post-DBS. This indicates the need for accurate assessment of non-dopaminergic disease
72 severity during the preoperative selection process.

73 Clinical, neuropsychological and psychiatric evaluations are used to rule out severe cognitive decline
74 or psychiatric comorbidity. However, several factors including intelligence, education, and
75 personality limit the interpretability of clinimetric assessments (Duncan, 1993). Moreover,
76 questionnaires and performance tasks are susceptible to misinterpretation, social desirability bias, or
77 fatigue (Duckworth et al. , 2015). Therefore, there is a need for complementary measures reflecting
78 disease severity in PD to aid the identification of DBS candidates.

79 Quantitative Electroencephalography (qEEG) is an inexpensive and widely available tool which
80 measures brain activity directly. Previous studies applied qEEG to examine clinical domains in PD,
81 such as cognition (Caviness et al. , 2015, Cozac et al. , 2016), response to treatment (George et al. ,
82 2013) or motor impairment (Babiloni et al. , 2011, George et al. , 2013). Global oscillatory slowing of
83 the EEG spectrogram is a highly suitable biomarker for cognitive impairment in PD (Caviness et al. ,
84 2015). Recent advances in neurophysiology have provided more complex markers such as

85 connectivity parameters and graph theory estimations, which quantify brain network disorganization.
86 The Phase-Lag Index (PLI), which reflects functional connectivity, was suggested as a potential
87 biomarker of PD dementia (Utianski et al. , 2016). To our knowledge the relation of qEEG parameters
88 to measures of non-dopaminergic severity in PD has not been investigated so far. We aimed to
89 investigate whether qEEG correlates with clinical measures of disease severity, in order to ultimately
90 provide neurophysiological determinants of disease severity.

91 **2. Methods**

92 **2.1 Study participants**

93 All consecutive PD patients who were referred for preoperative screening to the DBS centre of Leiden
94 University Medical Center (LUMC) and Haga Teaching Hospital between September 2015 and July
95 2017 were included in the study. All patients fulfilled the Movement Disorders Society PD criteria for
96 clinically established PD (Postuma et al. , 2015). Written informed consent was obtained from all
97 patients. A formal ethical evaluation of this study was waived by the local medical ethics committee.

98 **2.2 Outcome measures**

99 Motor function was assessed with the Movement Disorders Society Unified Parkinson's Disease
100 Rating Scale (MDS-UPDRS) part III (Goetz et al. , 2007) (range 0-132), whereas the SEverity of
101 Non-dopaminergic Symptoms in Parkinson's Disease (SENS-PD) scale quantified non-dopaminergic
102 disease severity (van der Heeden et al. , 2016) (range 0-54). The SENS-PD scale is a composite score
103 comprising three items with four response options (range 0-3) from each of the following six
104 predominantly non-dopaminergic domains: postural instability and gait difficulty (PIGD), psychotic
105 symptoms, excessive daytime sleepiness (EDS), autonomic dysfunction, cognitive impairment and
106 depressive symptoms (van der Heeden et al. , 2016). These six domains represent a coherent complex
107 of symptoms that is already present in early disease stages and increases in severity with age and
108 advancing disease. The SENS-PD scale is a recently developed, short, reliable and valid scale that
109 includes symptoms that do not improve with dopaminergic medication and may therefore more

110 accurately reflect severity and progression of the underlying disease than currently used dopamine-
111 sensitive measures. Higher scores on both the MDS-UPDRS III and SENS-PD scale reflect more
112 severe impairment.

113 Patients were subdivided a posteriori into three groups of comparable size, according to the tertile in
114 which their SENS-PD score fell: low disease severity (range 4-10), intermediate severity (range 11-
115 14) and high severity (range 15-24).

116 **2.3 EEG recording and pre-processing**

117 EEGs were recorded with patients lying supine, with eyes closed, during a state of relaxed
118 wakefulness. Light was kept at moderate intensity. Ag/AgCl EEG electrodes were placed on the scalp
119 using 21 standard 10-20 EEG electrode positions. Additional ECG and horizontal eye movement
120 leads were added for identification of artifacts. Data were acquired online using a Nihon Kohden
121 EEG-1200 system, with a 500 Hz sampling rate, a 16-bit analog-to-digital converter, and band-filtered
122 between 0.16 and 70 Hz. An EEG technician monitored signal quality throughout the entire recording;
123 patients were alerted by acoustic stimuli upon drowsiness. All patients used dopaminergic medication
124 according to their individual schedule.

125 **2.4 EEG analysis**

126 EEG data were re-referenced towards a source derivation which approaches the surface Laplacian
127 derivation (Hjorth, 1980). Five consecutive, non-overlapping 4096-point epochs lasting 8.192 seconds
128 were selected for further analysis after an artifact-free signal was visually confirmed. The individual
129 epochs were offline converted to American Standard Code for Information Interchange (ASCII)
130 format and further analysed using Brainwave software (BrainWave version 0.9.152.4.1, C.J. Stam;
131 available at <http://home.kpn.nl/stam7883/brainwave.html>). Recordings with less than five artifact-free
132 epochs were excluded from analysis. Analyses were performed in signal space to allow for direct
133 analysis of the raw EEG data in Brainwave software, which is easily reproducible for most clinicians
134 and may increase the utility of our findings.

135 Spectral analysis was performed off-line by processing each epoch with a Fast Fourier Transform
136 (FFT) and averaged to produce a power spectrum for each individual electrode. The frequency bands
137 were defined as δ (0.5 – 4.0 Hz), θ (4.0 – 8.0 Hz), α_1 (8.0 – 10.0 Hz), α_2 (10.0 – 13.0 Hz) and β (13.0
138 – 30.0 Hz). γ band power was not analysed due to frequent contamination with muscle artifacts.
139 Relative bandpower was calculated by dividing the absolute bandpower of each frequency band by
140 the total absolute bandpower from the FFT average per channel. Regional band powers were defined
141 as: frontal for F3, F4, F7, F8 and Fz, temporal for T3, T4, T5 and T6, parietal for P3, P4 and Pz,
142 central for C3, C4 and Cz, and occipital for O1 and O2. Global bandpower was defined as the average
143 of all regional band powers. A spectral ratio was calculated by dividing the sum of the relative power
144 in the δ and θ bands by the sum of the relative power in the α and β bands. These spectral bands were
145 selected a priori to incorporate as much of the EEG spectrum as possible, without contaminating the
146 results with possible artefacts that may be present in the fast frequency bands.
147 Functional connectivity was assessed by calculating the PLI in each frequency band. The PLI
148 quantifies phase coupling (range 0-1) whilst being insensitive to common sources and volume
149 conduction. PLI=0 indicates either no phase synchronization or equal in both leading and lagging
150 throughout the epoch, PLI=1 indicates perfect phase-locking (Stam et al. , 2007).

151 **2.5 Statistical analysis**

152 Baseline demographic, clinical, and test variables were not-normally distributed and were thus
153 compared between the three groups with Kruskal-Wallis H tests for continuous variables and
154 Pearson's χ^2 tests for dichotomous variables. Included and excluded patients were compared using
155 Mann-Whitney U tests. QEEG parameters were compared across SENS-PD tertiles using Kruskal-
156 Wallis H tests; Mann-Whitney U tests compared the high- and low-disease severity tertiles.
157 The association between the SENS-PD composite score, SENS-PD subdomains, MDS-UPDRS III
158 score and qEEG parameters was assessed by calculating partial Pearson's r correlation coefficients,
159 with an additional correction for age and usage of psychoactive medication, which may influence
160 EEG parameters. Bias-corrected and accelerated bootstrapping was performed with 7000 samples to
161 normalize the data; further increasing the amount of samples did not improve statistical accuracy.

162 Given the exploratory nature of our study, to avoid type II errors, no further correction for multiple
163 testing was applied. Missing values were imputed using multiple imputation with five iterations, if no
164 more than 15% of the data was missing.

165 All analyses were performed using IBM Statistical Package for the Social Sciences 23 Software
166 (SPSS Inc., Chicago, Illinois, USA). Significance was set at the 0.05 level. Graphical visualization of
167 results was performed in either MATLAB R2016A (The MathWorks Inc., Natick, Massachusetts,
168 USA) or GraphPad Prism 7.02 (GraphPad Software Inc., La Jolla, California, USA).

169 **3. Results**

170 **3.1 Patient characteristics**

171 Eighty patients underwent DBS screening during the study period. Seventeen patients were excluded
172 due to gross artifacts during EEG recordings (low disease severity: n=8, intermediate severity: n=3,
173 high disease severity: n=6); analysis was thus performed on 63 patients (32% female). There were no
174 significant differences in demographic and clinical variables between included and excluded patients.
175 Mean (SD) age was 62.4 (7.2) years, and disease duration 11.9 (6.3) years (table 1). There were no
176 significant differences in age, sex, disease duration, psychoactive drug usage and MDS-UPDRS III
177 score between the three SENS-PD tertiles. By design, both the SENS-PD score and all six subdomains
178 differed significantly between tertiles, with higher scores for the high-disease-severity group.

179 **3.2 Spectral analyses**

180 Slower EEG frequency bandpowers (i.e. δ and θ) were higher in the high-disease-severity group,
181 whereas faster frequency bandpowers (i.e. α_1 , α_2 and β) were higher in the low-disease-severity group
182 (Figure 1).

183 Mean spectral ratios (supplementary table 1) differed significantly between the high and low tertiles,
184 both globally and over the frontal, central, parietal and occipital regions. The high-disease-severity
185 group demonstrated a higher spectral ratio, indicating a greater proportion of slow EEG power.

186 The SENS-PD composite score showed a significant positive correlation with the spectral ratio: a
187 higher ratio, reflecting a greater proportion of slow EEG power, correlated with more severe non-
188 dopaminergic impairment, across all brain regions. The subdomains cognition and psychotic
189 symptoms showed significant correlations for all regions, whilst the subdomains PIGD and depression
190 showed a non-significant positive trend. The subdomains EDS, autonomic dysfunction and the MDS-
191 UPDRS III score did not correlate with EEG parameters (Figure 2).

192 **3.3 Functional connectivity**

193 Global PLI in the $\alpha 2$ band was significantly different between the three tertiles, while differences in
194 the other frequency bands were non-significant (supplementary table 2). Regional mean $\alpha 2$ PLI values
195 (supplementary table 3) differed significantly between the tertile groups over the frontal, central,
196 temporal and occipital regions. Patients in the high-disease-severity group had a lower connectivity
197 density, i.e. number of connections per threshold PLI value, than patients in the low-disease-severity
198 group (Figure 3), indicating that higher disease severity was associated with lower functional
199 connectivity.

200 Global, frontal, central, parietal and occipital PLI in the $\alpha 2$ band was significantly negatively
201 associated with the SENS-PD composite score and with the cognitive subdomain (supplementary
202 figures 1 and 2). The subdomain ‘psychotic symptoms’ showed a significant negative correlation over
203 the central electrodes and a negative trend over all brain regions. In all instances, reduced functional
204 connectivity correlated with higher disease severity.

205 **4. Discussion**

206 Several qEEG parameters were found to have potential as neurophysiological determinants of
207 advanced non-dopaminergic disease severity in PD. As high non-dopaminergic disease severity is a
208 relative contra-indication for DBS, qEEG analysis may ultimately complement clinimetric evaluations
209 to optimize the screening process of DBS candidates.

210 Slower EEG oscillatory activity was associated with more advanced non-dopaminergic disease
211 severity measured by the SENS-PD score and, in particular, with the subdomains cognition and
212 psychotic symptoms, with a trend towards a correlation with PIGD and depressive symptoms.
213 Conversely, the subdomains EDS and autonomic dysfunction did not show a clear pattern of
214 correlation. Motor impairment did not significantly correlate with spectral parameters.
215 Previous literature confirms the association between cortical slowing and cognitive impairment in PD
216 (Caviness et al. , 2015). The consistent EEG slowing both on a global level and across all the different
217 brain areas indicates diffuse dysfunction. It has been previously suggested that diffuse cortical
218 slowing in PD reflects a degeneration of a non-dopaminergic system with ascending cortical
219 projections (Olde Dubbelink et al. , 2013), which seems compatible with the observed correlation
220 between clinical measures of non-dopaminergic disease severity and EEG slowing.
221 Cortical slowing has been associated with severity of psychiatric symptoms also in other conditions.
222 In schizophrenic patients, auditory hallucinations were associated with task-related θ slowing (Zheng
223 et al. , 2015) and in cases with a delirium, visual hallucinations were associated with θ - δ slowing
224 (Teeple et al. , 2009). Although results of these studies based on other diseases may not be directly
225 comparable with PD, we speculate that these findings suggest a more general cortical
226 desynchronization, rather than network alterations that are specific to PD.
227 Reduced functional connectivity in the α 2 band significantly correlated with higher non-dopaminergic
228 disease severity, particularly with cognition, with a similar trend for the subdomains psychotic
229 symptoms, depression, PIGD and EDS. Motor impairment did not correlate with functional
230 connectivity. Only one EEG-study previously investigated PLI in PD, reporting reduced α 1 PLI
231 values in demented PD patients relative to cognitively normal PD patients. α 1 PLI likewise correlated
232 with the MMSE scale (Utianski et al. , 2016). Reduced α 1 PLI values were also found to correlate
233 with increased severity in Alzheimer's Disease (AD) (Engels et al. , 2015). Our results indicate a non-
234 significant trend for α 1 PLI, whereas we found α 2 PLI to be significantly reduced. This discrepancy
235 can be explained by a difference in population, as previous studies investigated patients with more
236 advanced cognitive deterioration while our population did not include demented PD patients, being
237 this a contra-indication for the DBS screening procedure. However, these findings suggest that

238 desynchronization of a similar α -band (either α_1 or α_2) network might underlie cognitive deterioration
239 in both PD and AD.

240 The described qEEG parameters, both oscillatory slowing and functional connectivity, demonstrate
241 discriminative ability at a group-level and may be further investigated to determine their potential as
242 biomarkers at an individual level.

243 Strengths of our study are the large sample size of consecutively included patients, standardized
244 examinations and use of a novel and validated clinimetric scale (SENS-PD). A limitation of the
245 SENS-PD scale is that the different subdomains may reflect different systems-at-risk, indicating that
246 similar scores between patients may reflect altogether different phenotypes, although this holds true
247 for any multidimensional scale including the MDS-UPDRS III. From a clinical perspective, not all
248 symptoms may be equally important, therefore the correlations with the SENS-PD scale were studied
249 both for the composite scores and its subdomains. Our study population consisted of potential
250 candidates for DBS. Typically, these patients had severe motor symptoms without obvious clinical
251 signs of cognitive dysfunction or psychotic symptoms. This homogeneity constitutes both a limitation
252 and a strength: although it is currently unknown whether our results can be generalised to all PD
253 patients, we show that qEEG is capable of quantifying subtle differences in patients with cognitive
254 and psychiatric symptoms that might go unnoticed in a global clinical impression. Investigations in a
255 wider range of PD patients at different disease stages are likely to show even more pronounced
256 correlations. Consequently, QEEG biomarkers for non-dopaminergic disease severity at different
257 disease-stages could have clinical applicability beyond DBS screening, such as monitoring of disease
258 progression.

259 The two applied methods of qEEG analysis do not show identical correlations with non-dopaminergic
260 domains, suggesting that they address different functional aspects. The negative association of cortical
261 connectivity in the α_2 band with cognitive impairment but the lack of correlation with the other non-
262 motor domains may reflect the subcortical nature of the latter. Whereas α -band connectivity is
263 associated with cognition, it is not specifically limited to cognition as evidenced by a non-significant
264 trend in the domain 'psychotic symptoms.' Although subcortical networks influence cortical
265 processes (Boon et al. , 2017), the exact subcortical alterations are not properly visualized by EEG

266 which accounts for the different results. Likewise, the lack of correlation between motor functioning
267 and EEG slowing provides further evidence that severity of motor impairment as assessed by the
268 MDS-UPDRS III is not reflected by cortical slowing (Babiloni et al. , 2011). Indeed, oscillatory
269 alterations in the (subcortical) basal ganglia, which correlate with motor dysfunction (Brittain et al. ,
270 2014), cannot be captured by EEG. Magnetoencephalography (MEG) could investigate these
271 subcortical networks (Boon et al. , 2017), however MEG is not widely available and is less applicable
272 for routine DBS screening purposes. Previous longitudinal studies using MEG have identified slowing
273 of oscillatory brain activities to be correlated with global disease progression in PD (Olde Dubbelink
274 et al. , 2013).

275 A limitation of the applicability of EEG as a biomarker is the proportion of excluded patients due to
276 EEG artifacts. These artifacts are partly inherent to the disease itself, such as altered muscle tone,
277 increased ocular movements, tremor, dyskinesias, and sleepiness. As baseline characteristics, both
278 motor and non-motor severity, did not differ between included and excluded patients, we expect that
279 the incidence of artifacts is not associated with disease severity. This is also confirmed by the fact that
280 in our cohort the number of recordings excluded because of artefacts was comparable in the low
281 disease severity group and high disease severity group.

282 Several factors might influence EEG activity, such as aging or use of psychoactive medication. For
283 this reason we corrected our results for both factors. Careful consideration of normal age-related
284 alterations cannot be neglected when assessing individual EEGs.

285 Changes of spectral- and connectivity parameters have also been found in epilepsy (Liang et al. ,
286 2010), AD (Engels et al. , 2015), and schizophrenia (John et al. , 2009) but it remains unclear whether
287 these disorders have a common cortical denominator or whether there are different disease-specific
288 network alterations.

289 EEG is available in every hospital, readily accessible and cheaper than other functional neuroimaging
290 measures such as MEG, fMRI, PET or SPECT (Lystad et al. , 2009). Moreover, source referencing
291 amplified the spatial resolution, overcoming criticism of EEG's limited resolution (Burle et al. ,
292 2015). Whereas the 21-channel EEG setup could be enhanced by using a high-density setup, we
293 demonstrated that conventional routine EEG is sufficient to provide parameters of non-dopaminergic

294 disease severity. Advanced setups do not seem necessary to achieve sufficient discriminative ability
295 on a group-level. In this study we demonstrate that disease severity is accurately reflected by both
296 functional connectivity and simpler EEG spectral measures, which are calculated with relative ease by
297 neurophysiologists. Future research could focus on validation in larger and more heterogeneous
298 cohorts to investigate whether qEEG may serve as biomarkers at an individual level, and determine its
299 accuracy in estimating disease severity. The use of EEG parameters to aid the selection process of
300 DBS candidates should also be further investigated.

301 In conclusion, we have demonstrated that both EEG slowing and reduced functional connectivity in
302 the $\alpha 2$ band are associated with increased non-dopaminergic disease severity in PD, particularly with
303 cognitive impairment and psychotic symptoms. These EEG alterations were apparent both globally
304 and over separate brain regions. The studied qEEG parameters may have the potential to ultimately
305 serve as complementary biomarkers of non-dopaminergic disease severity in PD.

306 **Authors disclosures and conflicts of interest**

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390

391 **Legends**

392 Figure 1. Distribution of the mean spectral powers per tertile of disease severity

393 *The high SENS-PD group demonstrated higher power in the slow EEG frequency bands (i.e. δ and θ);*
394 *the low SENS-PD group demonstrated higher power in the faster EEG frequency bands (i.e. $\alpha 1$, $\alpha 2$*
395 *and β), indicating a global slowing of EEG frequency with increasing disease severity (yellow: high*
396 *power, blue: low power).*

397

398 Figure 2. Correlation of slow-over-fast spectral ratio and disease severity

399 *Asterisks indicate significant correlations. A spectral ratio of slow-over-fast EEG power correlated*
400 *significantly with the SENS-PD composite score (i.e. more slow EEG power correlated with increased*
401 *non-dopaminergic disease severity). The subdomains psychotic symptoms and cognition correlated*
402 *significantly with the spectral ratio, whilst a trend could be observed for the subdomains PIGD and*
403 *depression. Error bars reflect 95% confidence intervals.*

404

405 Figure 3A. Connectivity density per tertile of non-dopaminergic disease severity (SENS-PD)

406

407 *Blue: low SENS-PD group, red: intermediate SENS-PD group, green: high SENS-PD group. The high*

408 *SENS-PD group demonstrated lower $\alpha 2$ PLI density than the low SENS-PD group, indicating a*

409 *reduction of functional connectivity with increasing disease severity. Network maps of the mean PLI*

410 *at three thresholds, i.e. $PLI=0.13, 0.15$ and 0.17 are shown in figure 3B.*

411

412 Figure 3B. Average network maps of the mean PLI in the $\alpha 2$ band per tertile of disease severity

413

414 *The $\alpha 2$ PLI network maps are plotted at three thresholds: $PLI = 0.15, 0.17$ and 0.19 . A line indicates a*

415 *level of functional connectivity of at least the threshold-value. With higher SENS-PD scores, the*

416 *threshold for functional connectivity is lowered, indicating a greater degree of cortical*

417 *desynchronization with increased disease severity.*

418 Supplementary figure 1. Correlation of global PLI values per frequency band and disease severity

419 *Error bars reflect 95% confidence intervals.*

420 Supplementary figure 2. Correlation of PLI in the $\alpha 2$ band and disease severity

421 *Error bars reflect 95% confidence intervals.*

422

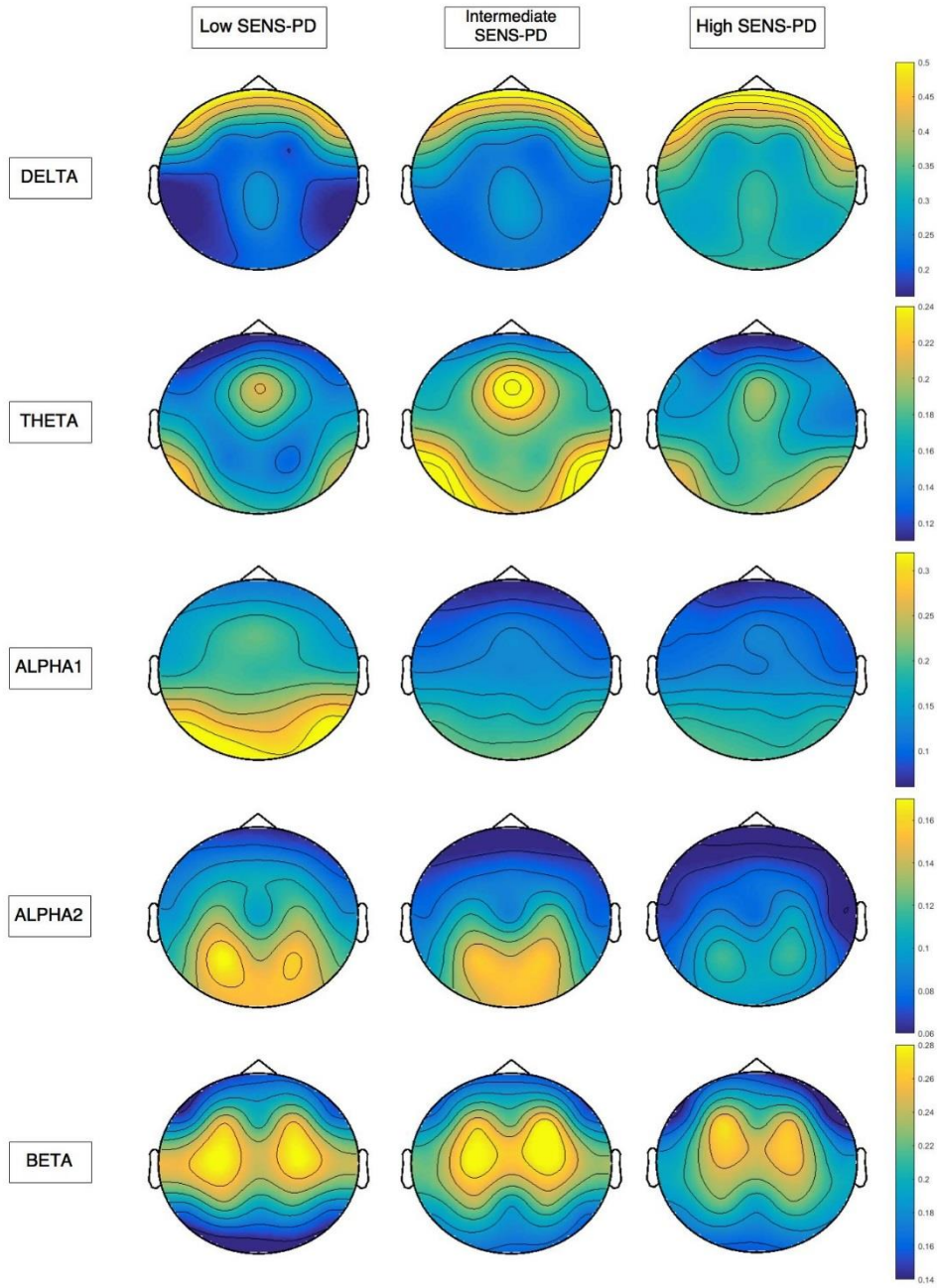
Table 1 Demographic and clinical characteristics

	Overall	Low SENS-PD	Intermediate SENS-PD	High SENS-PD	P
N	63	17	25	21	
EEG data, seconds	516.1	139.3	204.8	172.0	
Age, years	62.4 (7.2)	61.6 (6.4)	62.2 (7.5)	63.3 (7.5)	0.825
Female sex	20 (32)	6 (35)	8 (32)	6 (29.0)	0.906
Disease duration, years	11.9 (6.3)	10.6 (3.0)	12.0 (6.7)	12.9 (7.6)	0.718
Use of psychoactive drugs	15 (31)	3 (18)	5 (20)	7 (33)	0.448
MDS-UPDRS III total score	24.0 (10.1)	20.7 (9.2)	24.3 (11.1)	26.4 (9.1)	0.167
SENS-PD total score	13.1 (4.9)	7.6 (1.8)	12.0 (0.8)	18.8 (2.9)	<0.001^a
PIGD subscore	1.2 (1.0)	0.7 (0.8)	1.0 (1.0)	1.8 (0.8)	0.001^{b, c}
EDS subscore	2.7 (1.8)	1.8 (1.3)	2.1 (1.5)	4.1 (1.6)	<0.001^{b, c}
Depression subscore	2.4 (2.0)	1.1 (1.6)	2.1 (1.7)	3.6 (2.1)	0.001^{b, c}
Autonomic dysfunction subscore	2.1 (1.2)	1.4 (1.1)	2.0 (1.0)	2.8 (1.2)	0.002^c
Psychotic symptoms subscore	1.0 (0.9)	0.5 (0.5)	0.9 (0.7)	1.5 (1.1)	<0.001^{b, c}
Cognition subscore	4.0 (1.6)	3.0 (1.6)	4.0 (1.2)	4.8 (1.6)	0.002^c

Results are expressed as mean (SD) for continuous variables, n (%) for categorical variables.

^a Sig. difference between all three groups. ^b sig. difference between intermediate and high tertiles. ^c sig. difference between low and high tertiles

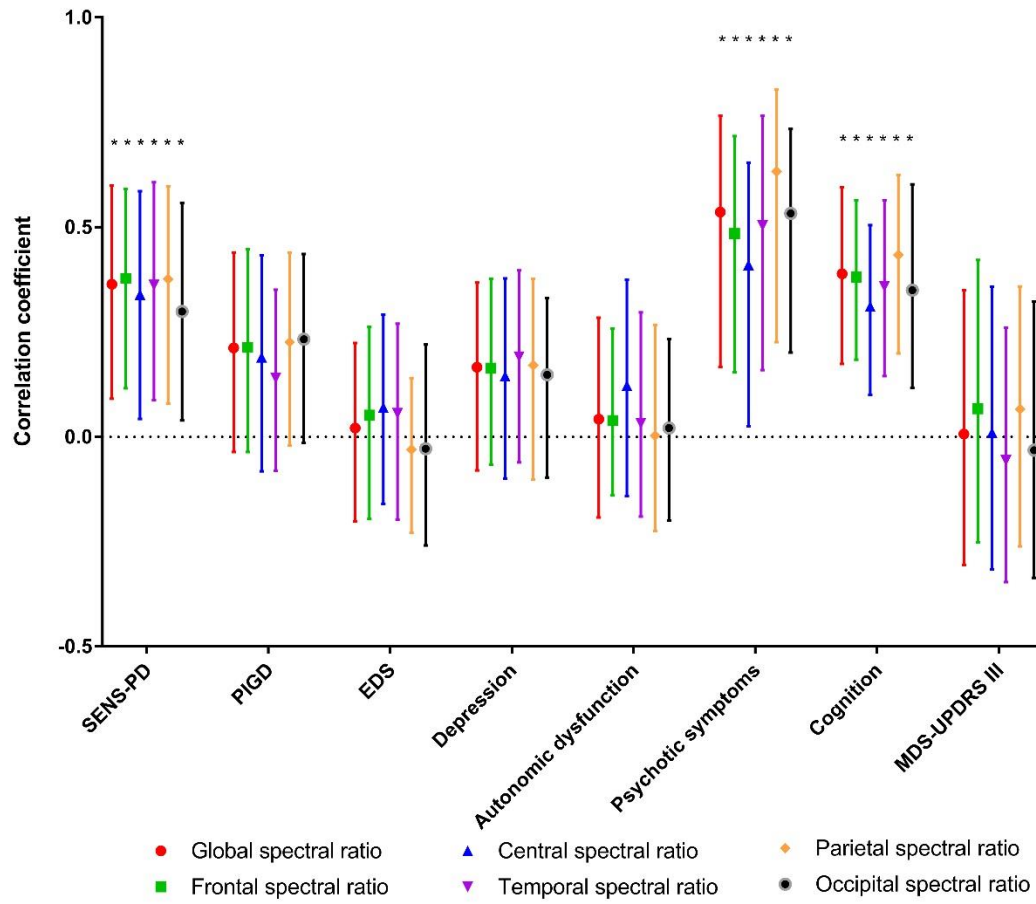
PIGD: postural instability and gait difficulty; EDS: excessive daytime sleepiness



424

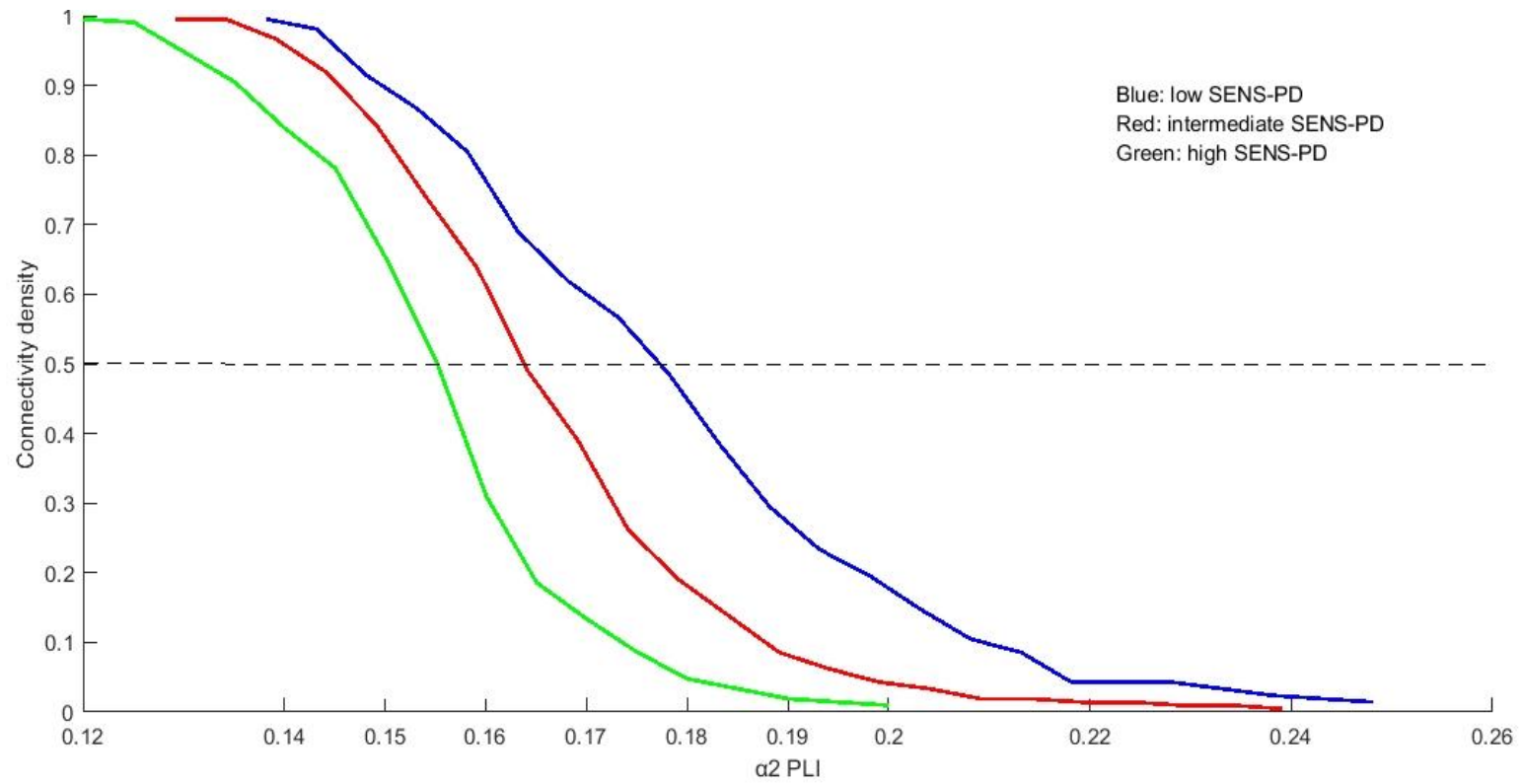
425 Fig 1.

426



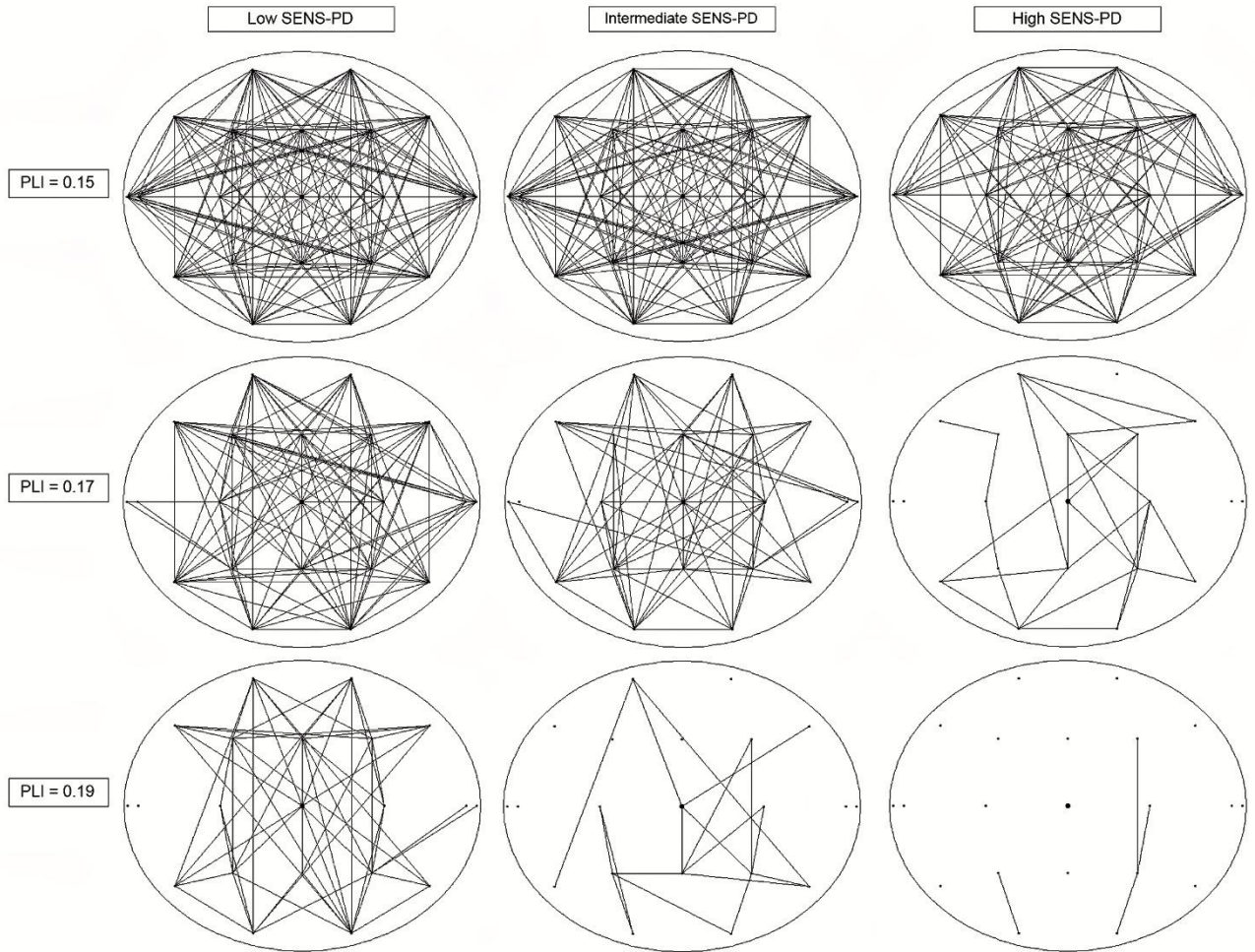
427

428 Fig 2.



429

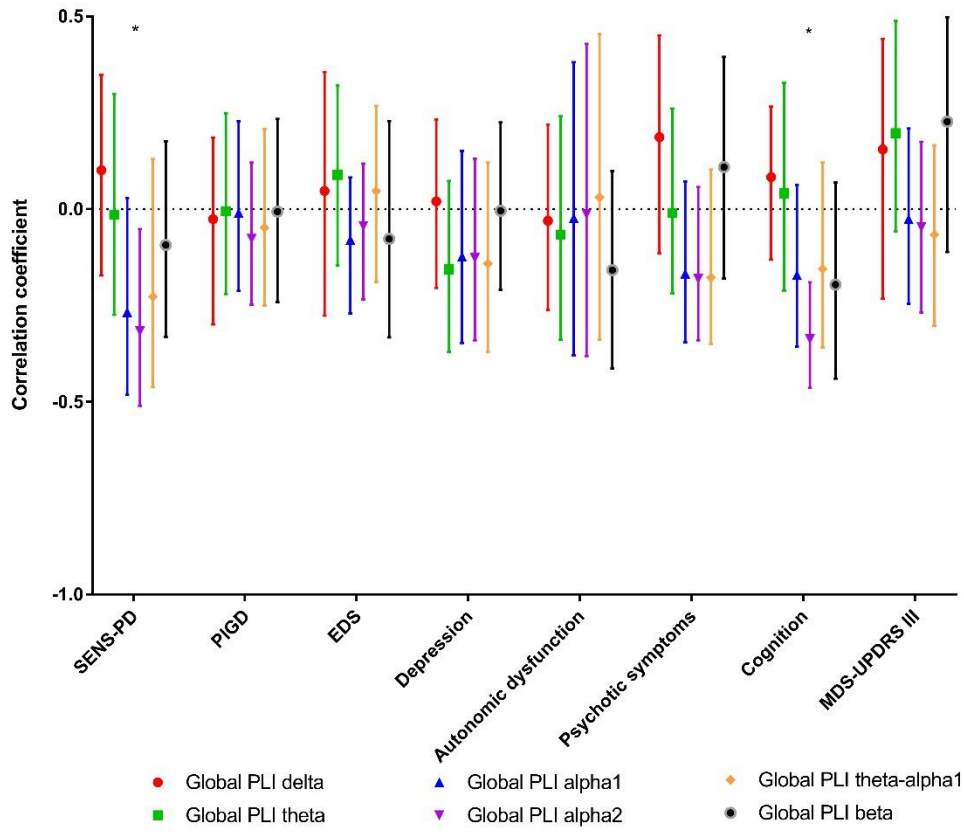
430 Fig 3A.



431

432 Fig 3B.

433

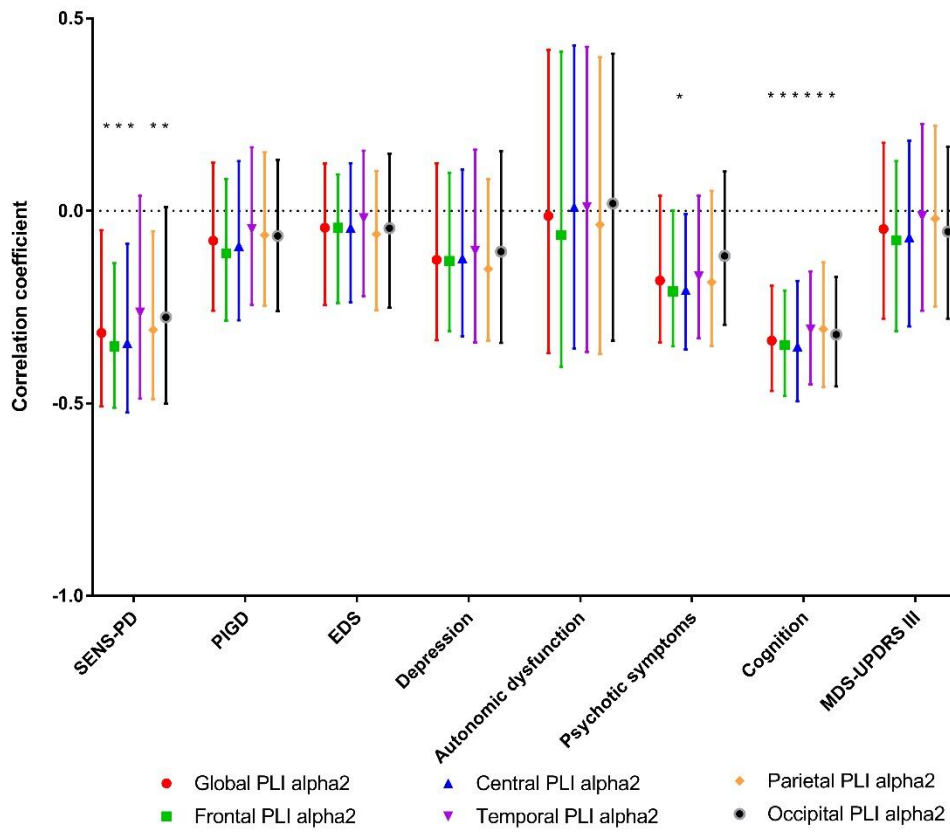


434

435 Supp. Fig 1.

436

437



438

439 Supp. Fig 2.