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Systems pharmacology of the amyloid cascade : unfolding oligomer modulation in Alzheimer's disease

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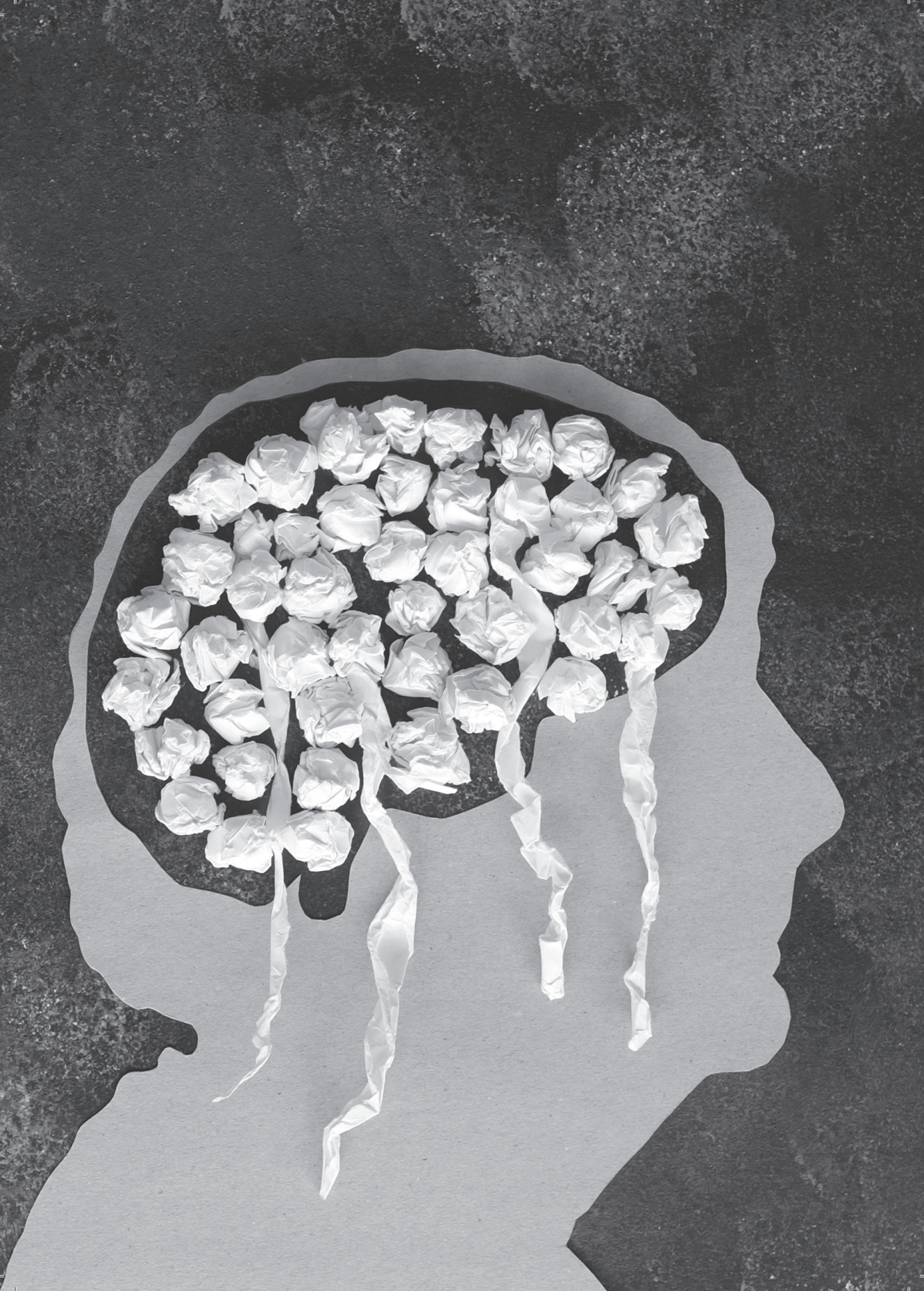


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Chapter 4

Integrating tracer kinetic data in a systems pharmacology model of the amyloid precursor pathway: effect of a β -secretase inhibitor

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Abstract

Purpose: To assess the ability of a recently developed systems pharmacology model of the β -amyloid precursor protein (APP) pathway to predict the tracer kinetics of APP metabolites following administration of a β -secretase inhibitor.

Methods: A stable isotope tracer $^{13}\text{C}_6$ -labelled Leucine was administered to cisterna magna ported (CMP) rhesus monkeys in conjunction with the β -secretase (BACE1) inhibitor MBI-5. The fraction labelled APP metabolites (total $A\beta$, sAPP α , sAPP β) were measured over 145 hours. A systems pharmacology model of the APP pathway, recently developed using information on CSF absolute concentrations of the APP metabolites ($A\beta_{40}$, $A\beta_{42}$, sAPP β and sAPP α), was used as the basis for the prediction of the tracer kinetic data.

Results: BACE1 inhibition by MBI-5 resulted in a concentration driven saturable effect on the APP pathway as reflected in the absolute concentrations of the metabolites, fraction labelled $A\beta$ and sAPP β . In contrast, this MBI-5 concentration dependency was not observed in the fraction labelled sAPP α because similar drug effects on both the labelled and unlabelled pools for this marker yield a lack of dose-differentiation in this relative biomarker. The recent APP systems model and absolute concentrations of the APP metabolites support a dose-dependent response. The current results indicate that interpretation of fraction labelled data is complex and best achieved with a kinetic model. $A\beta_{40}$ and $A\beta_{42}$ dynamics did not fully explain the measured fraction labelled $A\beta$. The model was used to demonstrate that a contribution of other $A\beta$ isoforms with altered dynamics from $A\beta_{40}$ and $A\beta_{42}$ is a potential explanation.

Conclusions: This analysis demonstrated that using a systems pharmacology model to integrate tracer kinetic data with absolute protein concentrations enables a more accurate interpretation of the tracer kinetic data.

Key words

Systems pharmacology - APP pathway - tracer kinetics - $A\beta$ - β -secretase inhibition

Introduction

The accumulation of amyloid- β ($A\beta$) peptide in the brain parenchyma as result of over-production and/or decreased clearance has been implicated in the pathophysiology of Alzheimer's disease (AD)¹. Toxic soluble $A\beta$ oligomers ($A\beta_O$) are considered to be the drivers of the neurodegeneration in the brains of patients with AD². Modulation of $A\beta$ is a therapeutic target for AD, with the potential for eliciting a disease modifying effect by reducing high levels of $A\beta$ peptides and subsequently preventing the development of $A\beta$ associated pathologies^{3,4}. One of the main therapeutic strategies aims at $A\beta$ reduction through the inhibition of secretases responsible for their production.

$A\beta$ peptides are generated by two sequential proteolytic cleavages of the β -amyloid precursor protein (APP)⁵. The first step is catalyzed by β -site APP-cleaving enzyme (BACE1, also called β -secretase) to yield the N-terminal fragment soluble APP β (sAPP β) and the C-terminal membrane-bound 99-aminoacid fragment (C99). C99 undergoes further cleavage by a second protease known as γ -secretase to generate $A\beta$ species of different chain lengths, the major variants having 38 ($A\beta_{38}$), 40 ($A\beta_{40}$) or 42 ($A\beta_{42}$) amino acids⁶. A third protease, α -secretase, cleaves APP within the $A\beta$ sequence generating non-amyloidogenic soluble APP α (sAPP α) and precluding the formation of the major $A\beta$ variants⁷. A new APP processing pathway was recently reported by Willem et al. (2015), in which sequential cleavage of APP by η -secretase and BACE1 or ADAM10 leads to the formation of $A\eta - \beta$ and $A\eta - \alpha$, respectively. There may be other alternate pathways unknown at this time.

To improve the prediction of therapeutic effects on $A\beta$ burden, an understanding of the behaviour of the APP system as a whole, as opposed to the behaviour of its individual components, is imperative. This requires a quantitative analysis of the dynamic interactions between drugs and the APP processing pathway. To this end, a systems pharmacology model of the APP processing pathway was reported recently⁹.

The model was based on the absolute concentrations of APP metabolites sAPP α , sAPP β , $A\beta_{40}$ and $A\beta_{42}$ and described their kinetics and interrelationships following β -secretase inhibition. In the current analysis, we evaluated whether the systems pharmacology model could adequately describe the tracer kinetic data of the APP metabolites following β -secretase inhibition.

Tracer kinetic studies have been introduced to gain understanding of the dynamics of the APP pathway following secretase inhibition. In 2007 Bateman et al.¹⁰ published a stable isotope labeling kinetics (SILK) protocol for quantification of $A\beta$ production

and clearance rates in the brain. In short, a tracer is infused intravenously after drug administration and the proportion of synthesized labelled APP metabolites is monitored for 145 hours. The SILK protocol measures the fraction of APP metabolites labelled with tracer. In addition, many of the SILK studies used liquid chromatography/MS or enzyme linked immunosorbant assay (ELISA) to measure absolute APP metabolite concentrations^{11,12,13}. Integrating the tracer kinetic data with absolute protein concentration measurements yields detailed insights in the functioning of the underlying biological system. For example, tracer kinetics combined with absolute protein concentrations have led to observations such as increased rates of the production of $A\beta$ in carriers of the PSEN1 mutation and a reported dose-dependent decrease in $A\beta$ production with γ -secretase inhibitors in humans^{11,14}. The technique has also been applied to define a clear related change in slowed $A\beta$ half-life and increasing age¹².

The objective of the current investigation is to compare the findings of the novel systems pharmacology model of the APP pathway to the tracer kinetic data. To this end, we extended the recently developed systems pharmacology model, by accounting for tracer dynamics throughout the APP pathway. Such an approach involves a quantitative analysis of the drug concentrations, plasma tracer enrichment and biomarker responses (absolute and fraction labelled proteins) using a comprehensive mathematical model that describes the underlying biological processes, while making a strict distinction between drug-specific and systems specific parameters. This allows for detailed interpretation of the biomarker responses by accounting for interdependencies among biomarkers as well as allowing for separation of rate *versus* extent of effects on the system. In this manner invaluable information is obtained on the functioning of the integrated biological system.

Dose ranging, biomarker, plasma tracer enrichment and pharmacokinetic data obtained from cisterna magna ported (CMP) rhesus monkeys receiving single doses of the BACE1 inhibitor MBI-5 and an infusion of the stable isotope tracer $^{13}\text{C}_6$ -labelled Leucine ($^{13}\text{C}_6$ -L) were available. The biomarkers measured were APP metabolites ($A\beta_{40}$, $A\beta_{42}$, sAPP β and sAPP α); their concentrations were determined by ELISA. SILK was utilized to determine plasma enrichment $^{13}\text{C}_6$ -L and fraction $^{13}\text{C}_6$ -L labelled APP metabolites (fraction labeled sAPP β , fraction labeled sAPP α , fraction labeled total $A\beta$).

The application of a systems pharmacology model based analysis accounting for tracer dynamics throughout the APP pathway revealed the similarities and differences in response measurements to BACE1 inhibition as determined by ELISA and SILK and these are discussed in this manuscript.

Materials and Methods

Animals

The CMP rhesus monkey model was described by Gilberto et al. (2003). The rhesus monkeys are chronically implanted with catheters in the cisterna magna, allowing repeated sampling of CSF and plasma. Six male animals, weighing between 5.2 and 11.7 kg (average, 8.7 kg), age 2 to 10 years (average, 8 years), were included in the study. Data from one animal was excluded from the analysis because of problems with the GS-MS.

These monkeys were captive-bred in a closed colony and individually housed. Animal use procedures were conform to the Guide for the Care and Use of Laboratory Animals¹⁶.

In vivo labeling protocol

The ¹³C₆-Leucine infusion protocol was previously described by Cook et al. (2010). In brief, the monkeys were administered ¹³C₆-labelled Leucine (¹³C₆-L) intravenously, with a primed infusion of 4 mg/kg bolus over 10 minutes, followed by 12 h of continuous infusion at a rate of 4 mg/kg/h. The primed 12 h ¹³C₆-L infusion was administered 1 hour post drug administration. The study protocol was described previously by Dobrowolska et al. (2014). CSF was sampled at -21, -19, 0 (pre-drug dose) and 3, 5, 7, 9, 13, 16, 19, 22, 25, 28, 31, 49, 55, 58, 73 and 145 h post drug administration, resulting in 19 samples for each monkey per treatment group to determine fraction labeled total A β , fraction labeled sAPP α and fraction labeled sAPP β . Blood was sampled at 0 (pre-drug dose) and 3, 5, 7, 9, 13, 16, 19, 22, 25, 28, 31 and 49 h post drug administration resulting in 13 samples for each monkey per treatment group to assess the ¹³C₆-L enrichment in plasma.

GC-MS was used to quantify plasma ¹³C₆-L enrichment as previously described by Bateman et al. (2007) and Cook et al. (2010). ¹³C₆-L enrichment was quantified as a tracer-to-tracee ratio (TTR).

A β , sAPP α and sAPP β were isolated by immunoprecipitation. To isolate A β a combination of the antibodies W0-2, directed against A β 5-8, and HJ5.1, raised against A β 13-28, was used. The proteins were proteolytically cleaved into smaller peptide fragments. LC-ESI-tandem MS was used to quantify the amount of ¹³C₆-L labeling in total A β , sAPP α and sAPP β at each time point. Fraction ¹³C₆-L labelled protein was calculated as the fraction of the signal intensities for labelled peptide fragments over the sum of the signal intensities for labelled and unlabelled peptide fragments¹⁷. For A β , the peptide quantified was A β ₁₆₋₂₇.

Drug administration and sampling

In a single dose, four-way, full crossover study, MBI-5 was administered at 10, 30, 125 mg/kg (5 mL/kg), or vehicle (0.4% methylcellulose) PO, with at least two weeks washout between each period. In conjunction $^{13}\text{C}_6\text{-L}$ was administered as described above. Plasma and CSF drug concentrations were collected at 0 (pre-drug dose) and 3, 5, 7, 9, 13, 16, 19, 22, 25, 28, 31, 49, 55, 58, 73 and 145 h post-drug dose, resulting in 17 plasma and CSF PK samples for each monkey per treatment group. 2 mL of blood and 1 mL of CSF were collected at each time point. The concentration of MBI-5 in the plasma and CSF samples was determined using LC-MS/MS. The pharmacological profile of MBI-5 was summarized by Dobrowolska et al. (2014).

The concentrations of $\text{A}\beta_{40}$, $\text{A}\beta_{42}$, $\text{sAPP}\alpha$ and $\text{sAPP}\beta$ were collected at -22, -20 and -1 h (pre-drug dose) and 2, 4, 6, 8, 12, 15, 18, 21, 24, 27, 30, 48, 54, 57, 72 and 144 h post-drug dose, giving 19 measurements of each biomarker for each monkey per treatment. 1 mL of CSF were collected at each time point. The assays used for the protein concentration measurements were described previously^{18,19,20}. Neopeptide-specific antibodies were used to detect $\text{A}\beta_{40}$ and $\text{A}\beta_{42}$, directed against $\text{A}\beta_{1-40}$ and $\text{A}\beta_{1-42}$.

PK-PD analysis

The PK-PD model has been developed and fitted to the data by means of non-linear mixed effects modelling using the NONMEM software package version 7 level 2²¹. The NONMEM software package was implemented on an Intel QuadCore (Intel® Core™ i7-3370 CPU, 3.40 GHz, 4.00 GB RAM) and Compaq Visual Fortran (version 6.6, Compaq Computer Corporation, Houston, Texas, USA) was used as compiler.

Modeling techniques were detailed by Van Maanen et al⁹. A decrease of 10.8 points in the minimum value of the objective function by adding an additional parameter, corresponding to $p < 0.001$ in a χ -squared distribution, was considered significant. Data management and model assessment were done using the statistical software package S-PLUS for Windows (TIBCO Spotfire S+® 8.2, TIBCO Software Inc.).

To validate the model a visual predictive check (VPC) was performed in which the median and the 90% inter-quantile range of the data simulated with the developed model were plotted together with the observations. A validated result is close agreement of median observed and predicted line with ~90% of the observations falling within the 90% prediction interval.

Model description

The systems pharmacology model of MBI-5 was based on sequential analysis of plasma tracer enrichment, PK and PD data. For the description of plasma enrichment over time a model that considers two pools for both $^{13}\text{C}_6\text{-L}$ and $^{12}\text{C}_6\text{-L}$ was developed (see Supplemental Material 1). The model related tracer input ($^{13}\text{C}_6\text{-Leucine}$ infusion, in mg/kg/hr) to the measured enrichment (tracer to tracee ratio, TTR in%) in plasma. The PK model of MBI-5 was based on simultaneous analysis of plasma and CSF PK data (see van Maanen et al. (2016)). The PK profiles of MBI-5 observed in plasma and CSF were adequately described, thus the model could serve as input for PD model analysis.

The PKPD model accounting for labelled and unlabelled species is an extension of the model presented in van Maanen et al. (2016). For each individual monkey, the PK of MBI-5 and kinetics of plasma tracer enrichment were utilized as two independent inputs, by using individual parameter estimates of the respective kinetic models. The biomarker response profiles of MBI-5 measured in CSF were adequately described by a model containing expressions to describe the time courses of APP, sAPP β , sAPP α , A β 40, A β 42, A β _O, FactorX (Fig. 4.1). sAPP β , sAPP α , A β 40 and A β 42 were informed by data, whereas APP, A β _O and FactorX were inferred based on the model and the data of aforementioned biomarkers. FactorX represents other (unknown) analytes quantified in fraction labelled A β (*vide infra*).

The production of APP was believed to be zero order, i.e. a constant production of APP. It was assumed that there is no alternative proteolytic enzyme cleaving full length APP other than α -secretase and BACE1. As both sAPP β and C99 are products of APP cleavage by BACE1, sAPP β and C99 were assumed to follow the same kinetics and therefore sAPP β could be used in the model as surrogate precursor for A β . The production of sAPP α , sAPP β and A β were assumed to be first order, i.e. dependent on the concentration of its precursor. To keep track of tracer dynamics throughout the pathway, two differential equations were implemented for each variable to account for labelled and unlabelled species, in which the tracer is assumed to be metabolically indistinguishable from the tracee. The system of differential equations is presented in Supplemental Material 4. The label incorporation in the APP pathway is driven by the kinetic model of plasma enrichment (Supplemental Material 4, Eq. S4.8 and S4.9). The inhibition of the BACE1 cleavage by MBI-5 was described by a sigmoidal I_{max} function (Supplemental Material 4, Eq. S4.22) using the individual predicted target site concentration of MBI-5, derived from the PK model (Supplemental Material 4, Eq. S4.23), as driver of the response.

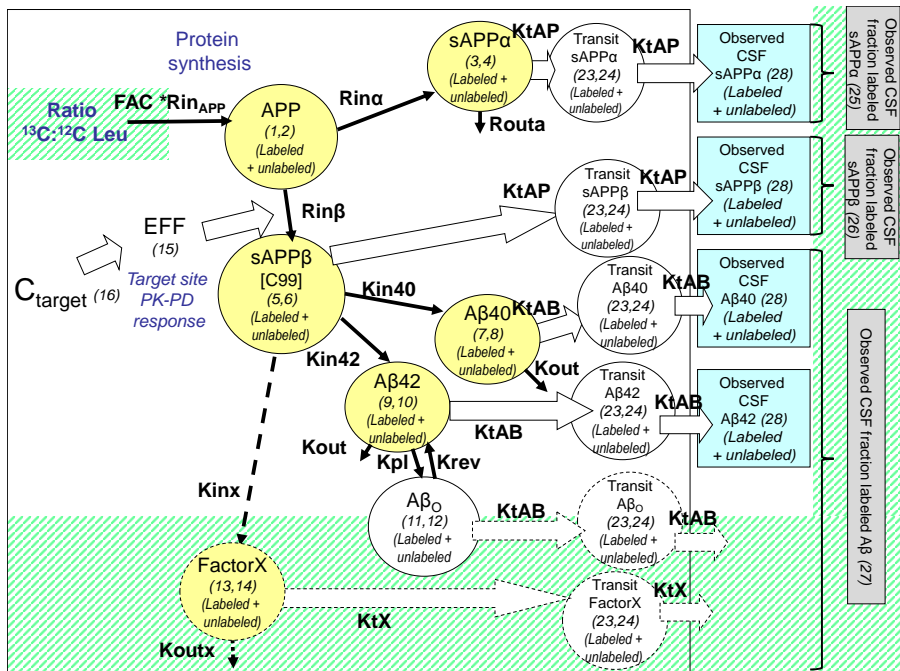


Figure 4.1: Schematic of systems model of APP processing.

The model comprised two times thirteen compartments: Six biomarker compartments in brain (yellow circles), one oligomer compartment and six transit compartments from brain to CSF (white circles), where each compartment was duplicated to track labelled and unlabelled species. Four biomarkers were measured in CSF (sAPP α , sAPP β , A β 40 and A β 42), indicated by the blue boxes. Total concentrations (labelled plus unlabelled) of sAPP α , sAPP β , A β 40 and A β 42 were measured using ELISA. Using SILK, fraction labelled sAPP α , fraction labelled sAPP β and fraction labelled total A β were determined where fraction labelled total A β is labelled over total A β species. The drug effect (*EFF*) inhibited *Rin β* . C_{target} , derived from the PK model, was used as driver of the biomarker response in the model⁹. sAPP β was used in the model structure as a surrogate substrate for C99 in the γ -secretase cleavage step. The tracer PK model of label enrichment of the Leucine pool (see Supplemental Material 1) informed label incorporation into the APP pathway.

Dashed arrows and compartments are additions to the model structure compared to the model based on ELISA data only⁹. Model extensions are indicated with the green shaded area. Equation numbers for each compartment have been included inside parentheses in order to facilitate their identification (see Supplemental Material 4).

APP: A β -precursor protein; *A β* : amyloid- β -peptide; C_{target} : drug concentration target site; *Kin*₄₀: A β 40 formation rate; *Kin*₄₂: A β 42 formation rate; *Kinx*: FactorX formation rate; *Kout*: A β 40 and A β 42 degradation rate; *Koutx*: FactorX degradation rate; *Krev*: Oligomer dissociation rate; *KtAP*: transit rate sAPP α and sAPP β from brain to CSF; *Kpl*: Oligomerization rate; *KtAB*: transit rate A β from brain to CSF; *RinAPP*: source of APP; *Rin β* : sAPP β formation rate; *Rin α* : sAPP α formation rate; *Rout*: sAPP β degradation rate; *Routa*: sAPP α degradation rate.

Results

Tracer enrichment in the brain

A kinetic model was used to describe the time course of the tracer enrichment in plasma during and after the infusion of the tracer. The model described tracer ($^{13}\text{C}_6\text{-L}$) and tracee (endogenous $^{12}\text{C}_6\text{-L}$) kinetics (see Supplemental Material 1).

Individual parameters from the kinetic tracer enrichment model were used to derive the enrichment at the target site in the brain. For this, the following assumptions were made: (1) there is no significant time delay between when the tracer is measured in plasma and when the tracer enters the brain. Any modest time delays in tracer entering the brain would be accounted for by later delay functions such as transit to CSF as the model could not independently assess this component of delay; (2) the shape of the enrichment-time profile in the brain is similar to that in plasma; (3) the probability of the incorporation of $^{13}\text{C}_6\text{-L}$ into protein is the same as the probability that endogenous $^{12}\text{C}_6\text{-L}$ is incorporated into protein; (4) none of the tracer incorporated into protein reappears as a consequence of protein breakdown in the time course of the tracer infusion. In the initial phase of tracer infusion the $^{13}\text{C}_6\text{-L}$ incorporation in the APP metabolites is so small, that it is unlikely that $^{13}\text{C}_6\text{-L}$ would be recycled by protein breakdown. Furthermore, protein turnover is assumed to be slow relative to the tracer infusion time.

No distinction can be made between the relative uptake of $^{13}\text{C}_6\text{-L}$ in the APP pool and the transport of tracer from plasma to the brain. The blood-brain barrier transport is assumed not to be the rate-limiting step for $^{13}\text{C}_6\text{-L}$ uptake in the APP pool. The relative formation of labelled and unlabelled APP species is related to the brain enrichment. Therefore, brain enrichment refers to the tracer ($^{13}\text{C}_6\text{-L}$) to tracee (endogenous $^{12}\text{C}_6\text{-L}$) ratio (TTR [%]) at the target site in the brain accessible for precursor (APP) formation. Consequently, brain enrichment can be derived using information from the placebo groups: if no inhibitor is given, and hence the system is in steady state, the sum of the labelled and unlabelled species is constant. A scale correction factor (*FAC*, see Supplement Material 4 Eq. S4.9) was applied to the plasma tracer enrichment, representing the relative uptake of tracer in the precursor (APP) pool. *FAC* was estimated to be 0.764 indicating that enrichment in the precursor pool was 76.4% of the level of plasma tracer enrichment.

Extension of the APP pathway model to account for tracer dynamics

Previously, a comprehensive systems model, incorporating the pharmacokinetics of MBI-5 and APP metabolites ($A\beta_{40}$, $A\beta_{42}$, sAPP α and sAPP β) concentrations was developed⁹.

The model quantified APP metabolite concentrations response to BACE1 inhibition and included an $A\beta_O$ compartment that could account for the differential effect of MBI-5 on $A\beta_{40}$ and $A\beta_{42}$ response. $sAPP\beta$ was used in the model structure as a surrogate substrate for C99 in the γ -secretase cleavage step. As $sAPP\beta$ and C99 are both products of the same cleavage step, their formation rates should be the same. Modeling efforts to separately account for $sAPP\beta$ and C99 did not improve the model description of the data and, therefore, demonstrated adequacy of the surrogate assumption.

For the current analysis, this model was extended to account for tracer dynamics throughout the APP pathway (Figure 4.1). The $^{13}C_6$ -L label incorporation into the APP pathway is determined from the derived brain tracer enrichment. To account for labelled and unlabelled species, two compartments were implemented for each variable (APP, $sAPP\beta$, $sAPP\alpha$, $A\beta_{40}$, $A\beta_{42}$, $A\beta_O$). Accordingly, the absolute amount of each APP metabolite is the sum of its labelled and unlabelled species and the fraction labelled APP metabolite is the ratio of labelled over the sum of its labelled and unlabelled species, with the exception of $A\beta$ (Supplemental Material 4, Eq. S4.32-S4.34). In the SILK protocol no distinction was made between $A\beta_{40}$ and $A\beta_{42}$. Therefore, fraction labelled $A\beta$ was initially assumed to be equal to the fraction labelled of total $A\beta_{40}$ and $A\beta_{42}$.

At first, the model structure and parameter values were fixed to those identified recently on absolute APP metabolite concentration data⁹. The model was then used to predict the fraction labelled proteins (SILK). Here, underprediction was observed for fraction labeled $sAPP\beta$ (placebo, dose 30 and dose 125 mg/kg, Fig. 4.4C, 4.4O, 4.4U) and fraction labeled $sAPP\alpha$ (placebo, 10 mg/kg, 30 mg/kg, Fig. 4.4A, 4.4G, 4.4M). Overprediction was observed for fraction labeled $A\beta$ for all dose groups (Fig. 4.4E, 4.4K, 4.4Q, 4.4W). As the response measurements to BACE1 inhibition by ELISA and SILK were the result of inhibiting the same pathway step, difference in effects of BACE1 inhibition on the biomarkers was not expected. Therefore, the flawed model fit indicated that there was additional information content to be gained from the SILK data beyond that from the ELISA. As such this additional data helped to better refine the true mechanistic representation of the APP system.

Accounting for differences in APP metabolite response measurements by ELISA and SILK

Integrating kinetic modelling of labelled and absolute data allows for the inconsistency of the results to be more robustly evaluated beyond comparison of observed response measurements. The results indicated a inconsistency between response magnitudes by

ELISA and SILK within the framework of the previously established kinetic model. Likely, aspects misspecified would be related to how the label is incorporated into the pathway or in how the two quantitative measures related to each other.

It was hypothesized that differences in APP metabolite responses as measured by ELISA and SILK may be caused by some deeper compartment in the APP pathway that could not be identified based on ELISA data only. This could be an additional APP pool causing a release of labelled APP that feeds slowly into the system, or an C99 pool that gives a slow release of labelled C99 that feeds into the system. Inclusion of the additional APP pool in the model worsened the description of fraction labeled sAPP α (results not shown). This indicated that the cause of the discrepancy in measurements should be sought further down the APP pathway. It was not possible to identify an C99 model component based on the current dataset, with which it was not feasible to separate the γ -secretase cleavage step from sAPP β elimination⁹.

An understanding of the assay differences between SILK and ELISA could suggest another alternate explanation of the disconnect, as one technique may have measured analytes which the other did not. Possibilities include ELISA cross-reactivity to species which were not measured by the SILK method, e.g. η -secretase products⁸, or SILK measured alternative APP fragments in addition to sAPP α , sAPP β , A β 40 or A β 42. If the same analytes were measured in both methods, then fraction labeled A β (SILK) would be composed of labelled over total A β 40 and A β 42 species and absolute A β 40 and A β 42 protein concentrations (ELISA) would be the sum of its labelled and unlabelled species. If the analytes as measured in SILK differ from those in ELISA this assumption will not hold. Fraction labelled A β (SILK) is then composed of labelled over total A β 40, A β 42 and other analytes. Absolute A β 40 and A β 42 protein concentrations (ELISA) remain the sum of their labelled and unlabelled species. To address this, a FactorX compartment was incorporated in the model representing these other analytes.

It was investigated if the other analytes represented by FactorX have a similar degradation rate (K_{outx}) as A β 40 and A β 42 (K_{out}). The formation rate of FactorX (K_{inx}) was defined by steady state conditions and derived from the other parameters (Supplement Material 4 Eq. S4.29). As a result, K_{inx} had a different value than K_{in40} and K_{in42} . With the similar degradation rate and the derived formation rate of FactorX, the inclusion of FactorX in the calculation of fraction labeled A β had no impact on the fraction labeled A β curve (not shown). Because mathematically terms were canceled out in the calculation of fraction labeled A β including FactorX, the same fraction labeled A β as

based on only labelled over total A β 40 and A β 42 species was obtained. This indicated

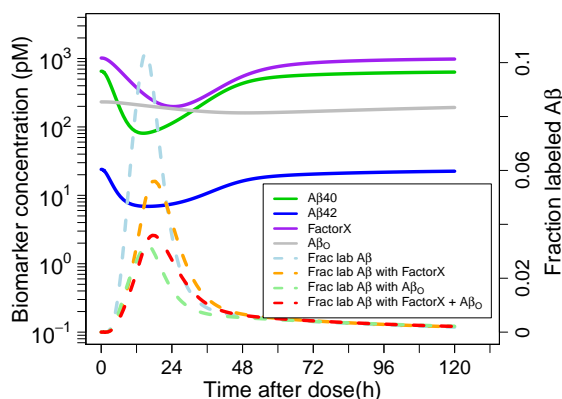


Figure 4.2: Graphical insight into the $A\beta$ biomarker responses in CSF, using the identified systems model of the APP processing pathway.

The biomarker responses in CSF are predicted after a single dose of 125 mg MBI-5, using the typical parameter estimates.

$A\beta_{40}$ green solid line; $A\beta_{42}$ blue solid line; FactorX purple solid line; $A\beta_0$ grey solid line; fraction labeled $A\beta$ light blue dashed line; fraction labeled $A\beta$ with FactorX orange dashed line; fraction labeled $A\beta$ with $A\beta_0$ light green dashed line; fraction labeled $A\beta$ with FactorX and $A\beta_0$ red dashed line.

that the analytes that were hypothesized to be additionally measured in SILK had to have different kinetics. Therefore, a different degradation rate for the analytes represented by FactorX was included in the model. The transit rate from brain-to-CSF for FactorX (KtX) was assumed to be similar to the transit rate for $A\beta$ species ($A\beta_{40}$ and $A\beta_{42}$). The model including FactorX labelled and unlabelled species, with different kinetics for FactorX than for $A\beta_{40}$ and $A\beta_{42}$, improved the description of the SILK data (results not shown). Description was further improved by also including labelled over total $A\beta_0$ in fraction labelled $A\beta$ as determined in CSF. For this, the transit of $A\beta_0$ from brain to CSF needed to be added to the model structure. This facilitated the identification of the $A\beta_0$ transit rate. When estimated the $A\beta_0$ transit rate was similar to the $A\beta$ transit rate from brain to CSF ($KtAB$) and could therefore be fixed to the same high value (10 h^{-1})⁹. It was not possible to identify the brain-turnover of $A\beta_0$ as a separate parameter. Therefore, the $A\beta_0$ half-life of 0.07 h reflects delays due to the brain-turnover and brain-to-CSF transfer. The value of the transit rate for sAPP α and sAPP β ($KtAPP$) should be interpreted relative to the $A\beta$ transit rate. By fixing $KtAB$ all possible delay is lumped in $KtAPP$.

The right panels in Fig. 4.4 show the description of the SILK data for the model with FactorX and $A\beta_0$ included in the calculation of fraction labelled $A\beta$. A prediction was performed with the model to investigate the contribution of FactorX and $A\beta_0$ to

the fraction labeled $A\beta$ curve (Fig. 4.2). The FactorX level was slightly higher than $A\beta_{40}$ and the shape of the FactorX response curve was different from the $A\beta_{40}$ and $A\beta_{42}$ responses due to the different degradation rate of FactorX (*Koutx*). Inclusion of FactorX and $A\beta_O$ in fraction labeled $A\beta$ had a lowering effect on the fraction labelled $A\beta$ curve and slightly altered its shape.

Comparison results based on ELISA and SILK versus ELISA only

Administration of MBI-5 increased $sAPP\alpha$ and decreased $sAPP\beta$, $A\beta_{40}$ and $A\beta_{42}$ concentrations in a concentration driven saturable effect as measured by ELISA (Fig. 4.5). A concentration-dependent response was also identified for the fraction labeled profiles of $A\beta$ and $sAPP\beta$. For the fraction labeled profile of $sAPP\alpha$, the drug effect was almost absent (Fig. 4.4). One single drug effect could describe the concentration-dependent response of all biomarkers, including the lack of response for fraction labeled $sAPP\alpha$.

Predictions from the systems model (Fig. 4.3) show that BACE1 inhibition resulted in a MBI-5 concentration driven accumulation of APP, leading to an increased production of $sAPP\alpha$ as APP is shunted down the α -secretase pathway. Both labelled and unlabelled species accumulate in a dose-dependent manner as result of BACE1 inhibition, but as the tracer infusion starts one hour post drug administration, the relatively more unlabelled species than labelled species accumulate. Due to the fractional nature of the fraction labeled measurement, these unlabelled species dilute the apparent response, from the start of drug treatment. Therefore, although there is a MBI-5 concentration driven increase in APP, this is not reflected in the 'fraction labeled APP' curve. The fraction labelled $sAPP\alpha$ is dependent on labelled APP and dilution by the accumulation of unlabelled $sAPP\alpha$. Consequently, minimal drug concentration-dependent increase appeared from the fraction labelled $sAPP\alpha$ curve, even though there is drug concentration driven increase in $sAPP\alpha$ formation. The same effect does not occur for fraction labeled $sAPP\beta$. The labeling process is continuous during the tracer infusion and washout, as is the APP accumulation during BACE1 inhibition. However, during the one hour time period between drug administration and start of tracer infusion there is no accumulation of unlabelled $sAPP\beta$, as $sAPP\beta$ levels are reducing as result of BACE1 inhibition. Therefore, there is no dilution of the apparent fraction labeled $sAPP\beta$ response by unlabelled $sAPP\beta$ species.

The drug potency (IC_{50}) identified in the combined analysis of ELISA and SILK data was $0.0267 \mu\text{M}$ (95% CI, 0.0201-0.0333), comparable to the IC_{50} identified on ELISA data only ($0.0269 \mu\text{M}$ (95% CI, 0.0154-0.0384))⁹. This value is also close to the *in vitro* inhibition constant (K_i) of 10 nM for MBI-5 inhibition of purified BACE1¹⁷. The Hill

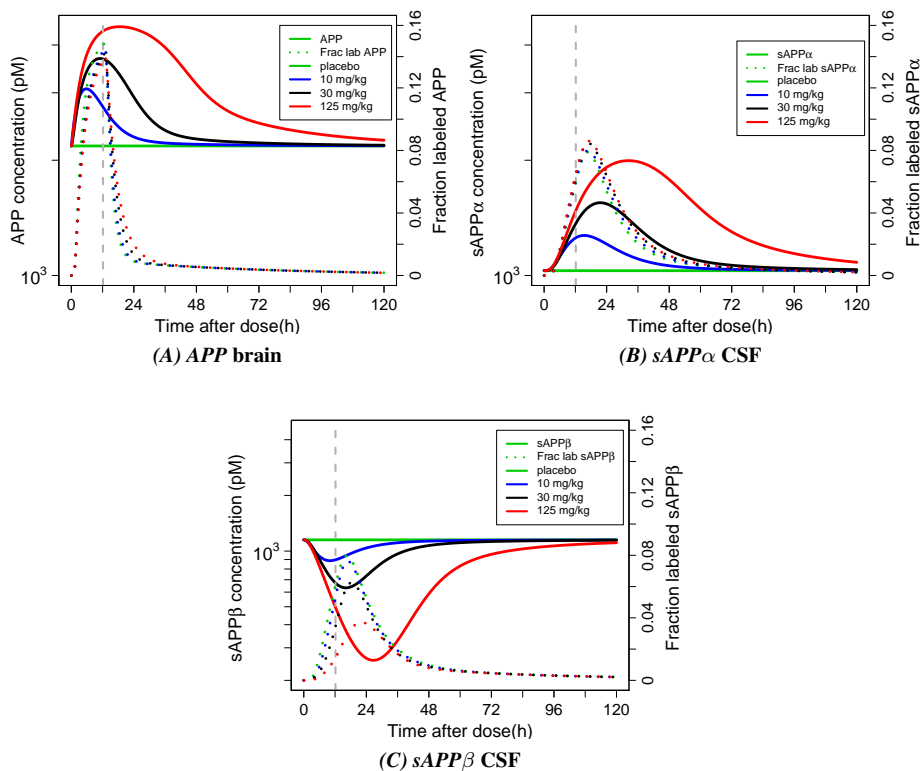


Figure 4.3: Predicted APP in brain (A), sAPP α in CSF (B) and sAPP β in CSF (C) responses, using the identified systems model of APP processing.

The biomarker responses are predicted after a dose range of MBI-5, using typical parameter estimates.

Absolute protein concentrations: solid line; Fraction labelled proteins: dotted line; Placebo: green; Dose 10 mg/kg: blue; Dose 30 mg/kg: black; Dose 125 mg/kg: red; End time of tracer infusion: vertical grey line.

coefficient of the concentration response relationship significantly changed from 1.53 (95% CI, 1.44-1.92) based on ELISA data to 0.986 (95% CI, 0.963-1.01) based on ELISA and SILK data. As the Hill coefficient was not significantly different from 1, the sigmoid-emax concentration response relationship could be reduced to an Emax relationship by fixing the Hill coefficient to 1. A Hill coefficient of 1 is the theoretical value for a simple receptor-target interaction. The shift to this value based on the ELISA and SILK data suggested that a more distinct representation of the inhibitor interaction with the target was achieved.

The Hill coefficient of unity based on ELISA and SILK data indicated a less steep

concentration response relationship than was identified on ELISA data only. Based on the ELISA and SILK data, inhibition rises much less quickly with concentration than expected based on the recent result. This mainly affected the description of the APP metabolite concentration response curves for the higher dose groups (Fig. 4.5)⁹.

The brain-turnover of sAPP α was slower based on the combined analysis (1.6 h) compared to based on ELISA data only (0.8 h). The identified proteolytic cleavage rates of APP by BACE1 and α -secretase imply that 49.1% of endogenous full length APP is cleaved by BACE1 and 50.9% by alternate pathways represented by the terms for α -secretase. These results are similar to the percentages APP identified to go down each path based on ELISA data only (44% and 56%, respectively)⁹.

A sequence of models with interanimal variability on different parameters was tested and the results compared, in order to select the best random effects model structure. The final model included interanimal variability on the baseline level of sAPP β and FAC. The identified interanimal variability on the baseline level of sAPP β also reflects on the baseline levels of the other APP metabolites, because of their interrelationships. Interanimal variability could not be identified for the drug effect parameters, indicating that the variation in drug effect was small relative to the underlying biologic variation in the system. Residual variability for absolute protein concentrations were implemented as proportional error models. Residual variability was higher for A β 40 and A β 42 than for sAPP β and sAPP α . Residual variability for fraction labelled proteins was implemented as an additive error model.

Table 4.1: Population parameter estimates including coefficient of variation (CV%) for updated model based on ELISA and SILK data.

PARAMETER	DESCRIPTION	VALUE	UNIT	CV%
<i>Structural parameters</i>				
sAPP β _{base}	baseline sAPP β	1.15e+003	pM	6.23
Fbase $A\beta$ ₄₀	A β ₄₀ baseline as fraction of sAPP β _{base}	0.566		7.83
Fbase $A\beta$ ₄₂	A β ₄₂ baseline as fraction of sAPP β _{base}	0.0208		5.58
Fbase _{sAPPα}	sAPP α baseline as fraction of sAPP β _{base}	0.895		2.20
Fbase _X	FactorX baseline as fraction of sAPP β _{base}	0.883		26.6
Rout _a	degradation rate sAPP α	0.427	h ⁻¹	5.53
Kout	degradation rate A β ₄₀ and A β ₄₂	0.603	h ⁻¹	7.05
Kout _x	degradation rate FactorX	0.138	h ⁻¹	9.78
KtAP	transit rate sAPP α and sAPP β	0.110	h ⁻¹	5.04
KtAB ^a	transit rate A β	10	h ⁻¹	
FAC	scale correction factor	0.764		2.50
Kpl	oligomerization rate	0.164	h ⁻¹	42.0
Krev	oligomer dissociation rate	0.0169	h ⁻¹	35.4
IM ^a	Imax	1		
IC50	IC50	0.0267	μ M	12.5
<i>Interanimal variability</i>				
ω^2_{BSAPb} ^b	Interanimal variability sAPP β baseline	0.0670		22.5
ω^2_{FAC} ^b	Interanimal variability scale correction factor (FAC)	0.0127		44.7
<i>Residual error</i>				
$\sigma^2_{A\beta 40}$ ^c	Residual variability A β ₄₀	0.266		15.4
$\sigma^2_{A\beta 42}$ ^c	Residual variability A β ₄₂	0.126		10.6
$\sigma^2_{\text{sAPP}\beta}$ ^c	Residual variability sAPP β	0.0548		14.6
$\sigma^2_{\text{sAPP}\alpha}$ ^c	Residual variability sAPP α	0.0625		8.19
$\sigma^2_{\text{FracLab}}$ ^c	Residual variability fraction labelled	4.62e-005		7.40

^a Fixed.

^b Interanimal variability is assumed to follow a normal distribution with mean zero and variance ω^2 .

^c Residual variability is assumed to follow a normal distribution with mean zero and variance σ^2 .

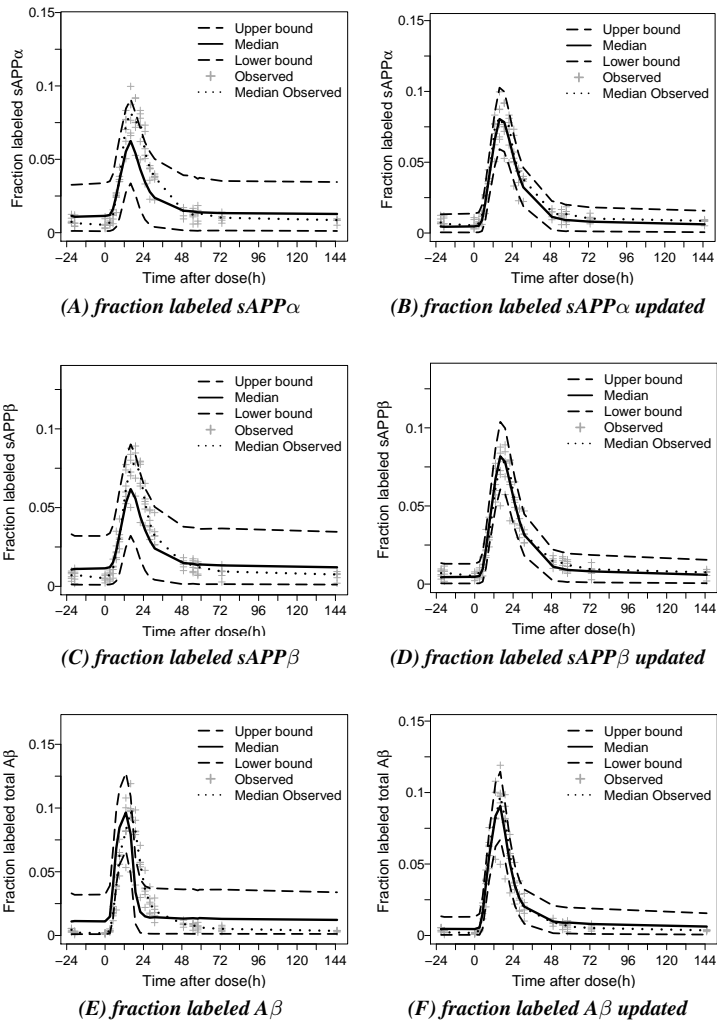


Figure 4.4: Visual predictive check of fraction labeled protein response vs. time profile of MBI-5 in the rhesus with 90% confidence interval.

Predictions were performed with model based on ELISA data only (*left*) and updated model based on ELISA and SILK data (*right*). Placebo (A-F), dose 10 mg/kg (G-L), dose 30 mg/kg (M-R) and dose 125 mg/kg (S-X). Observation sample size: $n=95$ for each SILK biomarker from 5 monkeys collected over 7 days at 4 occasions.

Solid line: Median model predicted fraction labeled protein response-time profile; *Long-dashed line*: 90 % prediction interval; *Dotted line*: Median observed fraction labeled protein response-time profile; *+ symbol*: Observations.

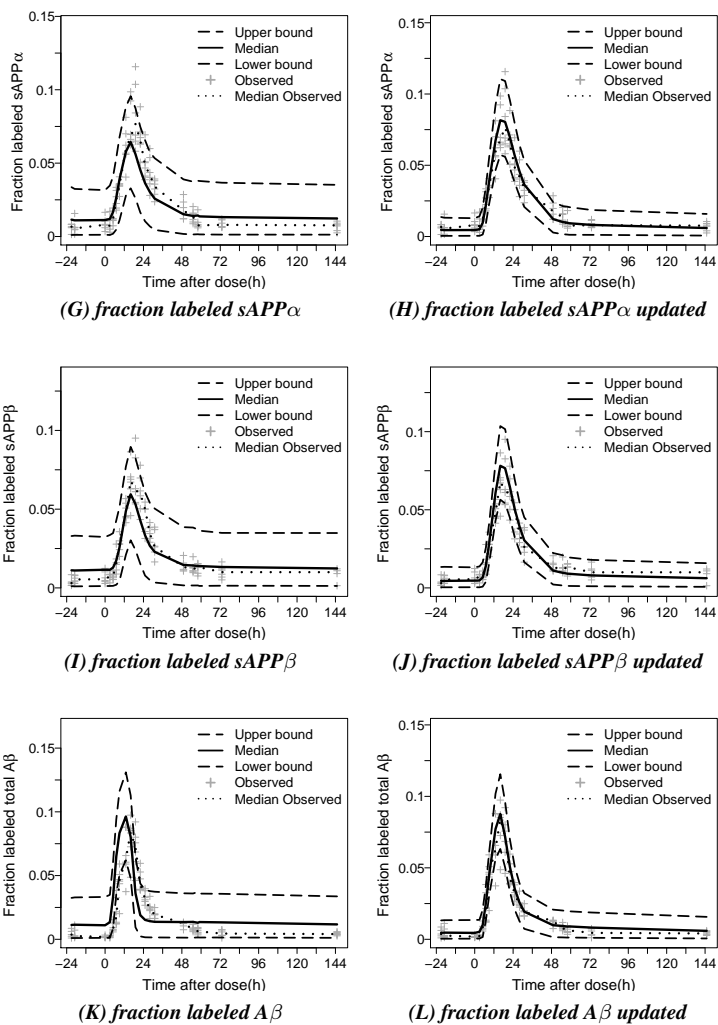


Figure 4.4: (Continued)

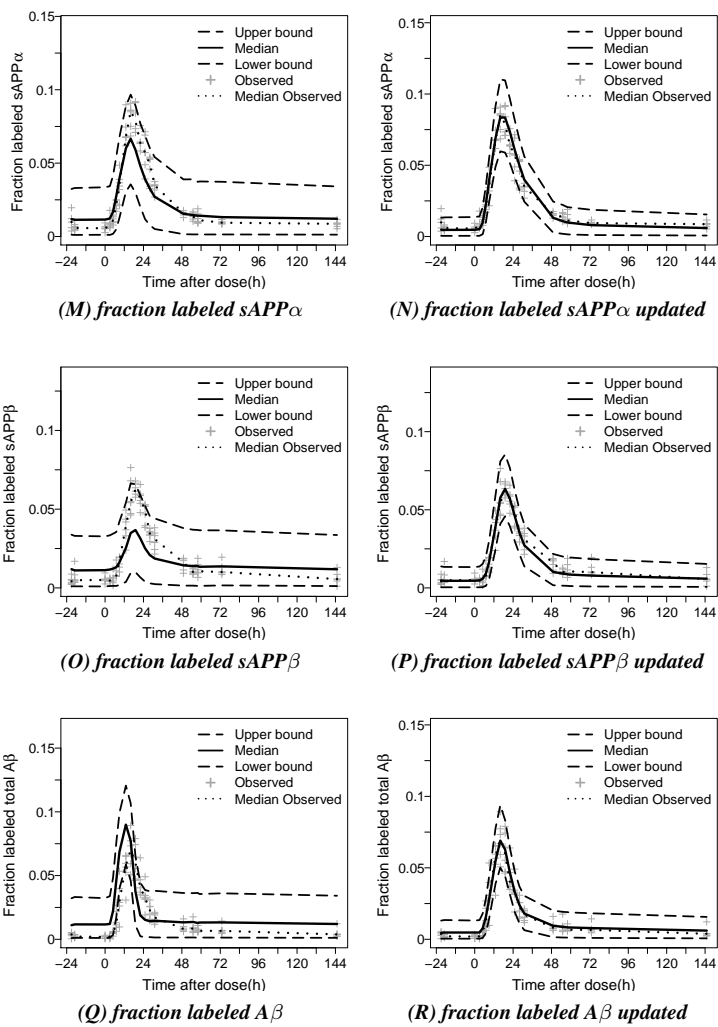


Figure 4.4: (Continued)

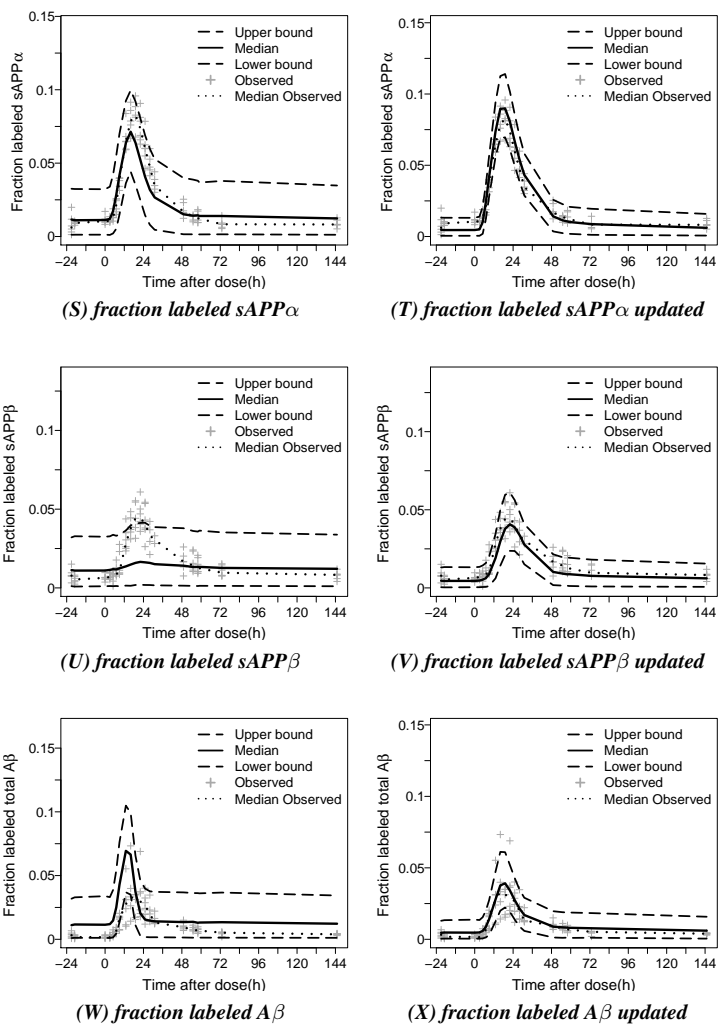


Figure 4.4: (Continued)

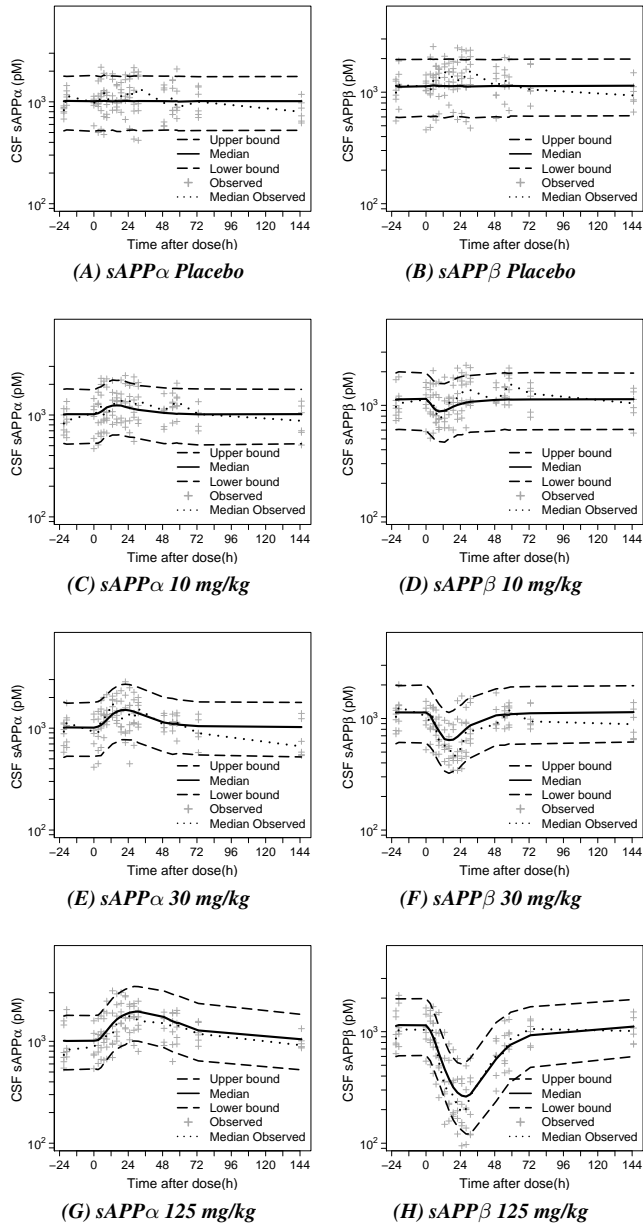


Figure 4.5: Visual predictive check of $sAPP\alpha$ (left: A,C,E,G), $sAPP\beta$ (right: B,D,F,H), $A\beta40$ (left: I,K,M,O) and $A\beta42$ (right: J,L,N,P) concentration response vs. time profile of MBI-5 in the rhesus with 90% confidence interval. Predictions were performed with updated model based on ELISA and SILK. Observation sample size: $n=95$ for each APP metabolite from 5 monkeys collected over 7 days at 4 occasions. *Solid line*: Median model predicted concentration-time profile *Long-dashed line*: 90 % prediction interval. *Dotted line*: Median observed concentration-time profile + *symbol*: Observations.

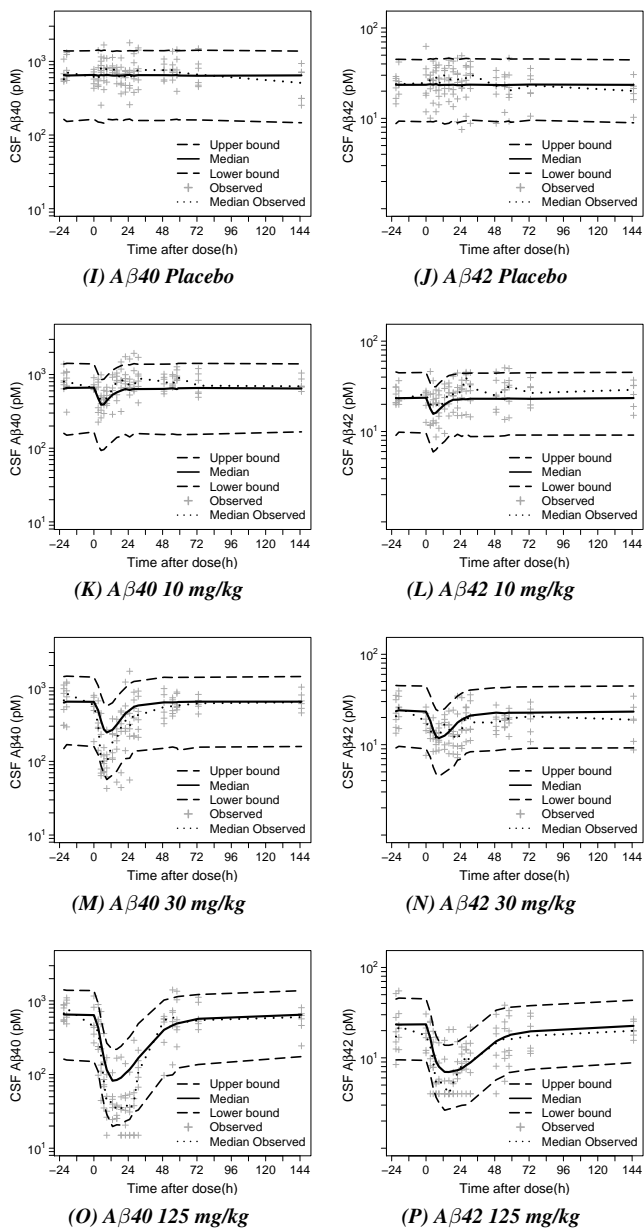


Figure 4.5: (Continued)

Discussion

Tracer kinetic studies are widely used to determine the influence of enzyme inducers or inhibitors on the rates of production and degradation of proteins. Traditionally, a non-compartmental analysis of the tracer enrichments versus time curve is used to estimate their effects on the rates of protein production and/or degradation. The rate of protein production being estimated from the upswing of the curve and the rate of degradation from the downswing. It has been demonstrated that the use of non-compartmental tracer kinetic data analysis where the enrichment is not in steady state could lead to inaccurate quantification of kinetic parameters²².

Alternatively, compartmental models have been used for this purpose^{23,24}. Here typically a standard two stage is followed in which each individuals PD parameters are estimated and then population mean and variance of each parameter are derived²⁵. A limitation of this approach is that the effect on protein disposition is related to the dose rather than to measures of drug concentrations.

To our knowledge, we are the first to utilize a population PK-PD modelling approach to the analysis of tracer kinetic data. The approach utilized here, in which the time course of the plasma tracer enrichment is analysed in conjunction with the time course of the plasma and CSF concentrations of the BACE1 inhibitor MBI-5, is novel for this type of data. The individual values of the (pharmaco)kinetic parameters obtained in these models serve as input for the modelling of the time course of the tracer enrichment of the APP metabolites. This enabled characterization of the concentration-enrichment-effect relationship of the BACE1 inhibitor, while taking into account the variability in PK, enrichment and PD in the study population.

We have recently been able to propose a systems pharmacology model for the APP processing pathway based on absolute concentrations of APP metabolites in rhesus monkeys⁹. This model provided a unique opportunity to further evaluate our understanding of the APP processing pathway while including tracer kinetic data in addition to absolute protein measurements. To this end we have simultaneously analysed the effects of a BACE1 inhibitor on the APP processing pathway, by analyzing the effects on tracer kinetic parameters (fraction labelled of various peptide species) as well as absolute protein concentrations. This has yielded invaluable information on the nature of measurements used in both techniques and on the underlying physiology.

The application of the existing systems pharmacology model to the combined dataset was generally consistent with our understanding of the APP processing pathway and

the existence of the oligomer pool. Moreover, the parameters describing the formation and degradation of the APP metabolites were comparable thereby strengthening our understanding of the relative contribution of the different analytes to the observed responses.

In the presence of the BACE1 inhibitor MBI-5 a concentration dependent saturable decrease in $A\beta_{40}$, $A\beta_{42}$ and $sAPP\beta$ concentrations was observed in combination with an increase in $sAPP\alpha$ absolute protein concentrations. In the SILK assay fraction labelled profiles for $A\beta$ and $sAPP\beta$ were reduced in a similar MBI-5 concentration-dependent manner. However, the effect on the fraction labelled profile of $sAPP\alpha$ was negligible. This is explained by the fact that the effect on $sAPP\alpha$ is an indirect effect through the accumulation of APP, secondary to the inhibition of BACE1. As the concentrations of both unlabelled and labelled $sAPP\alpha$ change in the same direction, there is no clear effect on the ratio labelled over total $sAPP\alpha$ (= the fraction labelled). This is further augmented by the fact that the tracer infusion starts one hour after MBI-5 administration. In this first hour after the administration of the BACE1 inhibitor unlabelled $sAPP\alpha$ starts to accumulate while there is no accumulation of labelled $sAPP\alpha$. This further dampens the effect on the fraction labelled $sAPP\alpha$. Finally, after a single dose of the BACE1 inhibitor, the observed dose response relationship also depends on the end time of the tracer infusion relative to the time of the maximal PD response.

In contrast to the attenuated effects of BACE1 inhibition on parameters characterizing the α -secretase pathway (fraction labelled $sAPP\alpha$), clear effects on the parameters of BACE1 pathway (fraction labelled $sAPP\beta$, fraction labelled $A\beta$) were observed, which is explained by the fact that these parameters are all downstream of BACE1, so that there is no accumulation of unlabelled protein in the time between drug administration and start of tracer infusion. These observations show, that due the complexity of the underlying biochemical network, lack of concentration dependent effect of an enzyme inhibitor on certain parameters, does not exclude the possibility that there is indeed such an effect.

We found a lower brain tracer enrichment relative to plasma tracer enrichment during $^{13}C_6$ -L infusion (Supplemental Material 3, Figure S4.4). The discrepancy between plasma tracer enrichment and target site enrichment may be explained by a lower amount of tracer at the target site, due to dilution of tracer. This may be the result of a higher amount of endogenous Leucine at the target site than in plasma. Also, kinetics of Leucine into and out of the cells, as well as into and out of the corresponding protein pools can differ across tissues ²².

The lower relative enrichment at the target site indicates that $^{13}C_6$ -L does not achieve

an isotopic equilibrium throughout all free pools of Leucine in the time frame of tracer infusion. This is also observed in the plasma tracer enrichment data, where plasma TTR is still rising during the 12 h infusion. This was confirmed by simulations using the developed model, indicating that it takes approximately 52 days of infusion to reach steady state with the primed-constant infusion technique as used in SILK (see Supplemental Material 1, Figure S4.3). With the primed 12 h infusion used in the current study, 62% of the steady state level of plasma tracer enrichment was reached. Therefore, the plateau observed in plasma tracer enrichment is a pseudo steady-state. The absence of steady state in tracer enrichment requires an analysis which takes into account the dynamics of the system, such as a comprehensive model based analysis performed currently.

The extension of the systems pharmacology model to include tracer kinetic data provides additional insights into the underlying APP processing pathway. Our modelling results indicate that 49.1% of APP is cleaved by BACE1 and 50.9% by α -secretase. It was assumed that all alternate pathways were represented by the terms for α -secretase. The reported percentage of APP to go down the α -secretase path should be interpreted as capturing the contribution of alternate pathways in general, as it acts to mediate the increase in APP which drives the α -secretase response and any other alternate pathway response. Increases in APP due to BACE1 inhibition result in more substrate being available to alternate pathways in general and α -secretase as an alternate path well represents this phenomena. It is expected that all alternate paths will behave dynamically as α -secretase does as all drug effects on alternate paths will be driven by the APP increase under BACE1 inhibition. The increases seen with α -secretase and captured in this model should also reflect the relative changes to be expected for any alternate pathway that may be present. Therefore, it is expected that sAPP- η would build-up in response to BACE1 inhibition similar to sAPP α build-up. An accumulation of the cleavage products of η -secretase after BACE1 inhibition was also reported by Willem et al 2015 in mice.

The simultaneous analysis of the combined data revealed differences in A β responses after BACE1 inhibition in rhesus monkeys as determined by ELISA and SILK. In a model-based analysis, in which knowledge of the biological system and analytical methods was integrated, various hypotheses to align APP metabolite response measurements in ELISA and SILK were tested. A possible explanation of the disconnect may be that an unknown process or analytes other than A β 40 (A β 1-40) and A β 42 (A β 1-42) were measured in SILK and not ELISA. The incorporation of the FactorX compartment in the model accounted for this (Fig. 4.1). The disconnect in measurements between both methods may be explained by the use of different measurement techniques. The antibodies

used in the ELISA where neoepitope-specific antibodies (N-terminal antibodies), directed against A β 1-40 and A β 1-42. The antibodies used to isolate A β in the SILK protocol were not end-specific for the N- or C-terminus, but directed against A β 5-27. As the antibodies used to isolate A β were raised against A β 5-27, these analytes that were detected in this assay must include this amino acid sequence.

A new APP processing pathway was recently reported by Willem et al 2015, in which sequential cleavage of APP by η -secretase and BACE1 or ADAM10 leads to the formation of A η - β and A η - α , respectively. Several A η peptides were reported by Willem et al 2015, that could have been captured by antibody W0-2, but not by HJ5.1, as used in the SILK protocol. Therefore, this does not explain the disconnect.

In an alternative path, BACE1 can cleave full length APP at the β -prime site (GLU11 in the A β sequence) leading to the production of A β 11-40 and A β 11-42. These are major cleavage products of BACE1, as reported by²⁶. Both A β 11-40 and A β 11-42 could not have been captured by the antibody W0-2 used in the SILK protocol, nor the neoepitope-specific antibodies used in the ELISA. Thus, β -prime site cleavage products cannot explain a difference in measurements between both methods.

It could be that ELISA does not detect the full complement of A β 42, as it is either tied up in A β _O or bound to a carrier protein²⁷. The methods used to detect the fraction labelled A β in the SILK protocol should also capture A β _O. How rapidly newly synthesized A β becomes an oligomeric species and how rapidly A β _O would move from brain to CSF is not known, but they are likely cleared to CSF much more slowly than the monomer due to their biophysical properties. It could also be that there is active transport of soluble toxic A β _O out of the brain, resulting in faster brain-to-CSF transport than for monomeric species. It was not possible to identify the brain-turnover of A β _O and turnover over brain-to-CSF transport as separate parameters. Therefore, the half-life of A β _O of 0.07 h reflects delays due to both brain-to-CSF transfer and turnover in the brain. Therefore, the rate of appearance of A β _O response in CSF relative to A β cannot be appointed to one of these processes.

Remarkably, different kinetics were identified for the process or analytes represented by FactorX, compared to A β 40 and A β 42. It was not possible to separate the rate of the γ -secretase cleavage from the brain-to-CSF transport. Therefore, the transit rates from brain-to-CSF for A β 40, A β 42 (KtAB) and FactorX (KtX) were fixed to an arbitrary high value (10 h⁻¹) and assumed to be equal.

Consequently, the A β 40 and A β 42 half-life of 1.1 h reflects delays due to the γ -secretase cleavage step and brain-to-CSF transfer. The current model structure in which

$A\beta_{40}$ and $A\beta_{42}$ are directly formed is a simplification of the underlying system. γ -secretase cleaves C99 through interactive pathways for stepwise successive processing to generate different $A\beta$ isoforms, with $A\beta_{40}$ and $A\beta_{42}$ as the major products²⁸. The initial γ -secretase cleavages are followed sequentially by γ -secretase cleavages after every three or four residues. The systems model was able to combine two types of data and describe seven biomarkers successfully. Adding the tracer kinetic data (SILK) to the model based on absolute protein concentrations (ELISA)⁹ confirmed the system that was identified on ELISA data only. This is one utility of the biomarkers of the SILK protocol. Our understanding of the relationships among the absolute APP metabolite concentrations did not change compared to the recent analysis based on ELISA data only. However, the combined analysis allowed for more hypotheses to be tested. Vice versa, including absolute protein concentrations in the interpretation of the tracer kinetic data had added value. This facilitated the correct interpretation of drug concentration dependencies in the tracer kinetic data and led to the investigation of a disconnect in the two type of measurements of the same system, which was accounted for by the FactorX model component.

If dedicated measurements of $A\beta_{1-40}$ and $A\beta_{1-42}$ were used in the SILK protocol, it is expected that $A\beta_{40}$, $A\beta_{42}$, fraction labelled $A\beta$ could have been described by a model without inclusion of the FactorX model component. However, even then, matrix components in the CSF may affect the measurement reproducibility across different immunoassays²⁷.

In a follow-up study, dedicated measures of $A\beta_{40}$, $A\beta_{42}$ and $A\beta_{38}$ will be performed in the same samples in both labelled and absolute quantification. In addition, $A\beta$ will be quantified using an antibody directed at the mid-domain $A\beta_{17-28}$. If FactorX is an $A\beta$ isoform, it would then be possible to determine if it has different half-lives from $A\beta_{40}$, $A\beta_{42}$ and $A\beta_{38}$ and how much FactorX accounts for total of $A\beta$ species compared to $A\beta_{40}$, $A\beta_{42}$ and $A\beta_{38}$.

Conclusion

This investigation demonstrated that the simultaneous analysis of absolute protein concentrations and tracer kinetic data using a systems pharmacology model will elucidate the underlying biological system and will thereby facilitate the interpretation of the tracer kinetic data in the light of the system. The model-based analysis distinguished labelled and unlabelled species, as well as separated steps in the APP pathway and distribution to CSF. This enabled and improved understanding of the (lack-of) dose-dependent response in kinetic data.

Different hypotheses to align APP metabolite response measurements in ELISA and SILK were tested. A possible explanation of the disconnect may be that an unknown APP fragment with differing kinetics or an unknown process was picked up in SILK assay. This requires further investigation.

The developed comprehensive model can be used to perform simulations to investigate study design features that may influence the magnitude of biomarker responses, such as dose and degree of $A\beta$ production inhibition. To maximize information on the APP pathway from the tracer protocol, simulations can be performed to investigate how the $^{13}\text{C}_6\text{-L}$ infusion time and length affects the fraction labelled curves (ongoing). It is anticipated that adding information on APP metabolite responses (absolute and fraction labelled proteins) following γ -secretase inhibition will provide more information on the biological system as well as the discrepancies between absolute protein concentrations and tracer kinetic data.

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Chapter 4

Supplemental Material

Supplement to

Integrating tracer kinetic data in a systems pharmacology model of the amyloid precursor pathway:
effect of a β -secretase inhibitor

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SUPPLEMENTAL MATERIAL (1)

Kinetic Data Analysis of Plasma Enrichment

A kinetic model was developed to quantify plasma $^{13}\text{C}_6\text{-L}$ enrichment in CMP rhesus monkeys. The results of the plasma enrichment analysis were included in the subsequent PK-tracer-PD analysis.

The kinetic model was developed and fitted to the data by means of non-linear mixed effects modeling using the NONMEM software package version 7 level 2 (see the Materials and Methods section in Chapter 4).

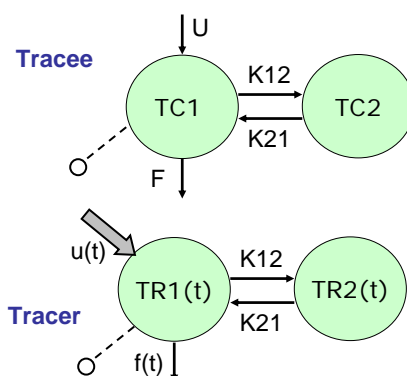


Figure S4.1: Model structure of kinetic model describing plasma tracer enrichment.

The model relates tracer input [mg/kg/hr] to the tracer-to-tracee ratio (TTR[%]). The model includes two tracee ($^{12}\text{C}_6\text{-Leucine}$) and two tracer ($^{13}\text{C}_6\text{-Leucine}$) compartments, representing extra- (pool 1) and intra-cellular (pool 2) tracee and tracer, respectively. Measurements are assumed to be taken from the extracellular compartment.

Dashed line: sampling. *Arrow:* tracer infusion. *U:* production of tracee in pool 1. *u(t):* tracer infusion into pool 1. *F:* disposal of tracee from pool 1. *f(t):* disposal of tracer from pool 1. *K12:* Transit rate from pool 1 to pool 2. *K21:* Transit rate from pool 2 to pool 1.

The compartmental model related the tracer infusion [mg/kg/h] to the measured enrichment, quantified as tracer ($^{13}\text{C}_6\text{-Leucine}$) to tracee (endogenous $^{12}\text{C}_6\text{-Leucine}$) ratio (TTR [%]), by describing tracee and tracer kinetics.

The model included two tracee ($^{12}\text{C}_6\text{-Leucine}$) and two tracer ($^{13}\text{C}_6\text{-Leucine}$) compartments (Supplemental Figure S4.1), representing extra- and intra-cellular tracee and

tracer. Measurements are assumed to be taken from the extracellular compartment.

Tracee is produced and disposed from tracee pool 1. Tracer is disposed from tracer pool 1. It is assumed that the natural production of tracer is negligible within the time frame of the experiment. The tracer coming into the system comes from the tracer infusion. The rate of disposal of tracer ($f(t)$) equals the rate of disposal of the tracee (F). The tracer and tracee kinetics is described by Eqs. S4.1 - Eqs. S4.4:

Tracee pool 1 (TC_1):

$$\frac{d}{dt}TC_1 = -K_{12} * TC_1 + K_{21} * TC_2 - F * TC_1 + U \quad (S4.1)$$

Tracee pool 2 (TC_2):

$$\frac{d}{dt}TC_2 = K_{12} * TC_1 - K_{21} * TC_2 \quad (S4.2)$$

Tracer pool 1 (TR_1):

$$\frac{d}{dt}TR_1(t) = -K_{12} * TR_1(t) + K_{21} * TR_2(t) - f(t) * TR_1(t) + u(t) \quad (S4.3)$$

Tracer pool 2 (TR_2):

$$\frac{d}{dt}TR_2(t) = K_{12} * TR_1(t) - K_{21} * TR_2(t) \quad (S4.4)$$

The TTR in plasma can then be calculated as described by Eqs. S4.5: Tracer to tracee ratio (TTR):

$$\frac{d}{dt}TTR = \frac{\frac{TR_1(t)}{TC_1} - TTR_{base}}{1 + 0.0111 * 6} * 100\% \quad (S4.5)$$

Here, TTR_{base} is the observed ratio of $^{13}C_6$ -Leucine to $^{12}C_6$ -Leucine prior to the addition of tracer.

The value $1/(1+0.0111*6)$ is the skew correction factor, accounting for the natural abundance of $^{13}C_6$ -Leucine¹. The spectrum of $^{13}C_6$ -Leucine does not have the same mass abundance distribution as natural $^{12}C_6$ -Leucine. In the calculation of TTR, this skew in

isotopomer distribution must be accounted for. The correction factor can be approximated by the value $1/(1+An)$, where A is the natural isotopic abundance of ^{13}C carbon atoms and n is the number of atoms labelled². 1.11% of the naturally occurring carbon atoms are ^{13}C atoms and Leucine has six carbon atoms ($\text{C}_6\text{H}_{13}\text{NO}_2$), therefore $1/(1+0.0111*6)$.

The baseline of tracee pool 2 ($TC_{2\text{base}}$) and production of tracee (U) follow from steady state conditions.

$$TC_{2\text{base}} = TC_{1\text{base}} * \frac{K_{12}}{K_{21}} \quad (\text{S4.6})$$

$$U = F * TC_{1\text{base}} \quad (\text{S4.7})$$

Supplemental Table S4.1 shows all kinetic parameter estimates. All parameters could be estimated with good precision. For the baseline of the tracee pool 1 ($TR_{1\text{base}}$) interanimal variability was quantified. The model included a proportional error to describe the residual variability.

The measured plasma tracer enrichment was adequately described by the model, as can be seen from the visual predictive check (Supplemental Figure S4.2). Thus, the model could serve as input for PK-tracer-PD model analysis.

Table S4.1: Population parameter estimates including coefficient of variation (CV%) for kinetic model of plasma tracer enrichment.

PARAMETER	DESCRIPTION	VALUE	UNIT	CV%
F	Disposal	0.931	h^{-1}	25.5
K12	Transit rate from pool 1 to pool 2	0.644	h^{-1}	16.5
K21	Transit rate from pool 1 to pool 2	0.0154	h^{-1}	33.4
$TC_{1\text{base}}$	Baseline tracee pool 1	141	mg	15.1
$\omega^2_{TC_{1\text{base}}}$	Interanimal variability baseline tracee pool 1	0.0166		20.0
σ^2	Residual variability	0.722		20.4

Time to steady state

A simulation was performed with the kinetic model to investigate if plasma tracer enrichment reached steady state with the primed 12 h $^{13}\text{C}_6\text{-L}$ infusion as used in the current SILK study (Supplemental Figure S4.3). To that end, the continuous infusion time was extended and the time to steady state derived. It takes approximately 52 days of infusion to reach steady state with the primed infusion technique. After approximately 10 and 17 days respectively 95% and 99% of the steady state level is reached. In the current study,

with the primed 12 h infusion, 62% of the steady state level of plasma tracer enrichment was reached.

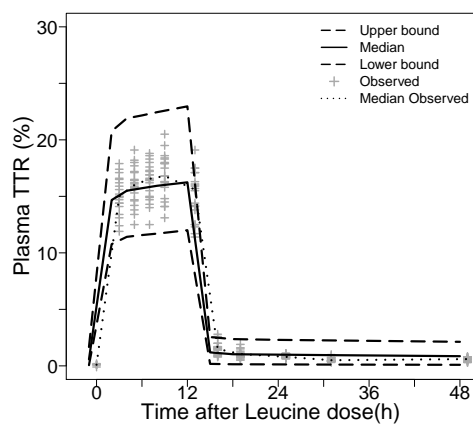


Figure S4.2: Visual predictive check of plasma tracer enrichment (TTR) time profile of $^{13}\text{C}_6$ -Leucine in the rhesus with 90% confidence interval.

Observation sample size: $n=260$ from 5 monkeys collected over 2 days at four occasions.

Solid line: Median model predicted plasma TTR-time profile *Long-dashed line:* 90% prediction interval.

Dotted line: Median observed plasma TTR-time profile *Plus-symbols:* Observations.

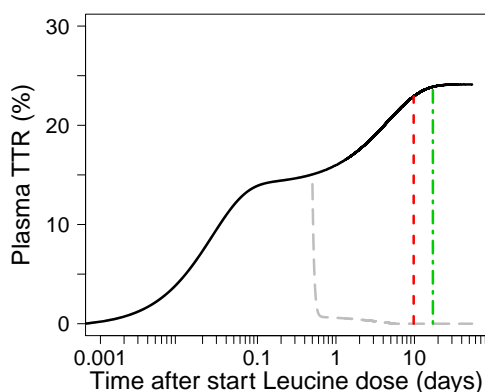


Figure S4.3: Simulation of plasma tracer enrichment (TTR) time profile using the identified kinetic model.

The plasma TTR is predicted after a primed infusion of 4 mg/kg bolus over 10 minutes, followed by 1300 h continuous infusion at a rate of 4 mg/kg/h, using the typical parameter estimates.

Steady state plasma TTR is reached after ~ 52 days of infusion.

Solid line: Model predicted plasma TTR-time profile after primed 1300 h infusion. *Long-dashed grey line:* Model predicted plasma TTR-time profile after primed 12 h infusion. *Dashed vertical red line:* Time of 95% steady state plasma TTR. *Dot-dashed vertical green line:* Time of 99% steady state plasma TTR.

References

1. Wolfe, R.R. & Chinkes, D.L. Isotope tracers in metabolic research: principles and practice of kinetic analysis 2nd ed. John Wiley & Sons; Hoboken, New Jersey; 2005.
2. Rosenblatt, J., Chinkes, D., Wolfe, M., & Wolfe, R.R. Stable isotope tracer analysis by GC-MS, including quantification of isotopomer effects. *Am J Physiol.* 1992;263(3 Pt 1):E584–96.

SUPPLEMENTAL MATERIAL (2)

Table S4.2: Population parameters derived from model parameters for updated model based on ELISA and SILK data.

PARAMETER	DESCRIPTION	VALUE	UNIT
$A\beta_{40}_{\text{base}}^{\text{a}}$	$A\beta_{40}$ baseline	650.9	pM
$A\beta_{42}_{\text{base}}^{\text{b}}$	$A\beta_{42}$ baseline	23.92	pM
$\text{FactorX}_{\text{base}}^{\text{c}}$	FactorX baseline	1,015	pM
$\text{sAPP}\alpha_{\text{base}}^{\text{d}}$	$\text{sAPP}\alpha$ baseline	1,029	pM
$A\beta_{\text{O}}_{\text{base}}^{\text{e}}$	$A\beta_{\text{O}}$ baseline	232.12	pM
$\text{APP}_{\text{base}}^{\text{f}}$	APP baseline	2,179	pM
$\text{Rin}_{\text{APP}}^{\text{g}}$	source of APP	9.25×10^{-7}	$\text{L}^{-1}\text{h}^{-1}$
$\text{Rin}_{\alpha}^{\text{h}}$	$\text{sAPP}\alpha$ formation rate	0.202	h^{-1}
$\text{Rin}_{\beta}^{\text{i}}$	$\text{sAPP}\beta$ formation rate	0.209	h^{-1}
$\text{Kin}_{40}^{\text{j}}$	$A\beta_{40}$ formation rate	0.341	h^{-1}
$\text{Kin}_{42}^{\text{k}}$	$A\beta_{42}$ formation rate	0.0125	h^{-1}
$\text{Kin}_{\text{x}}^{\text{l}}$	$A\beta_{\text{x}}$ formation rate	0.122	h^{-1}

$$^{\text{a}} A\beta_{40}_{\text{base}} = \text{Fbase}_{A\beta_{40}} * \text{sAPP}\beta_{\text{base}}$$

$$^{\text{b}} A\beta_{42}_{\text{base}} = \text{Fbase}_{A\beta_{42}} * \text{sAPP}\beta_{\text{base}}$$

$$^{\text{c}} \text{FactorX}_{\text{base}} = \text{Fbase}_{\text{FactorX}} * \text{sAPP}\beta_{\text{base}}$$

$$^{\text{d}} \text{sAPP}\alpha_{\text{base}} = \text{Fbase}_{\text{sAPP}\alpha} * \text{sAPP}\beta_{\text{base}}$$

$$^{\text{e}} A\beta_{\text{O}}_{\text{base}} = \text{Kpl} * A\beta_{42}_{\text{base}} / \text{Krev}$$

$$^{\text{f}} \text{APP}_{\text{base}} = \text{sAPP}\beta_{\text{base}} + \text{sAPP}\beta_{\text{base}}$$

$$^{\text{g}} \text{Rin}_{\text{APP}} = (\text{Rin}_{\alpha} + \text{Rin}_{\beta}) * \text{APP}_{\text{base}} * \text{MW}_{\text{LeuL}} / (\text{TC}_{1\text{base}} * 10^9)$$

$$^{\text{h}} \text{Rin}_{\alpha} = \text{Rout}_{\alpha} * \text{sAPP}\alpha_{\text{base}} / \text{APP}_{\text{base}}$$

$$^{\text{i}} \text{Rin}_{\beta} = (\text{Kin}_{40} + \text{Kin}_{42} + \text{Kin}_{\text{x}}) * \text{sAPP}\beta_{\text{base}} / \text{APP}_{\text{base}}$$

$$^{\text{j}} \text{Kin}_{40} = \text{Kout} * A\beta_{40}_{\text{base}} / \text{sAPP}\beta_{\text{base}}$$

$$^{\text{k}} \text{Kin}_{42} = \text{Kin}_{40} * A\beta_{42}_{\text{base}} / A\beta_{40}_{\text{base}}$$

$$^{\text{l}} \text{Kin}_{\text{x}} = \text{Kout}_{\text{x}} * \text{FactorX}_{\text{base}} / \text{sAPP}\beta_{\text{base}}$$

SUPPLEMENTAL MATERIAL (3)

Simulation scale correction factor

In the PKPD model the plasma tracer enrichment was scaled to the level of tracer enrichment in the brain using a scale correction factor FAC . FAC represents the relative uptake of tracer in the precursor APP pool and was estimated to be 0.764. $^{13}\text{C}_6\text{-Leu}$ does not achieve an isotopic equilibrium throughout all free pools of Leucine within the timeframe of the tracer infusion. Therefore, the tracer enrichment in the brain differs from plasma enrichment.

If isotopic equilibrium is assumed, and hence $FAC=1$, the fraction labelled protein is overestimated for fraction labelled total $A\beta$, $sAPP\beta$ and $sAPP\alpha$, as is demonstrated in Supplemental Figure S4.4 for the placebo group.

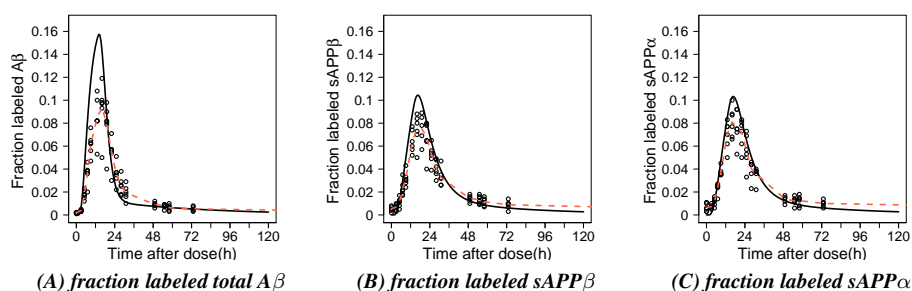


Figure S4.4: Simulation fraction labelled protein response vs. time profile for the placebo group with scale correction factor (FAC) equals 1.

Solid line: Predicted fraction labelled protein response-time profile; *Dashed line:* Smoother through the observations of the placebo group; *Symbols:* Observations placebo group.

SUPPLEMENTAL MATERIAL (4)

Equations

The interaction between labeled and unlabelled APP, sAPP β , sAPP α , A β ₄₀, A β ₄₂, A β _o and FactorX is described by Eq. S4.8 - Eq. S4.21:

$$\begin{aligned} \frac{d}{dt} APP^{unlab} = & Rin_{APP} * \frac{TC_1 * 10^9}{MW_{LeuU}} - (Rin\beta * EFF + Rin\alpha) * APP^{unlab} \\ & - Rin_{APP} * \frac{TR_1 * 10^9 * FAC}{MW_{LeuL}} \end{aligned} \quad (S4.8)$$

$$\begin{aligned} \frac{d}{dt} APP^{lab} = & Rin_{APP} * \frac{TR_1 * 10^9 * FAC}{MW_{LeuL}} \\ & - (Rin\beta * EFF + Rin\alpha) * APP^{lab} \end{aligned} \quad (S4.9)$$

$$\frac{d}{dt} sAPP\alpha^{unlab} = Rin\alpha * APP^{unlab} - Rout_a * sAPP\alpha^{unlab} \quad (S4.10)$$

$$\frac{d}{dt} sAPP\alpha^{lab} = Rin\alpha * APP^{lab} - Rout_a * sAPP\alpha^{lab} \quad (S4.11)$$

$$\begin{aligned} \frac{d}{dt} sAPP\beta^{unlab} = & Rin\beta * EFF * APP^{unlab} \\ & - (Kin_{40} + Kin_{42} + Kin_x) * sAPP\beta^{unlab} \end{aligned} \quad (S4.12)$$

$$\begin{aligned} \frac{d}{dt} sAPP\beta^{lab} = & Rin\beta * EFF * APP^{lab} \\ & - (Kin_{40} + Kin_{42} + Kin_x) * sAPP\beta^{lab} \end{aligned} \quad (S4.13)$$

$$\frac{d}{dt} A\beta_{40}^{unlab} = Kin_{40} * sAPP\beta^{unlab} - Kout * A\beta_{40}^{unlab} \quad (S4.14)$$

$$\frac{d}{dt} A\beta_{40}^{lab} = Kin_{40} * sAPP\beta^{lab} - Kout * A\beta_{40}^{lab} \quad (S4.15)$$

$$\begin{aligned} \frac{d}{dt}A\beta_{42}^{unlab} = & Kin_{42} * sAPP\beta^{unlab} - Kout * A\beta_{42}^{unlab} \\ & - Kpl * A\beta_{42}^{unlab} + Krev * A\beta_O^{unlab} \end{aligned} \quad (S4.16)$$

$$\begin{aligned} \frac{d}{dt}A\beta_{42}^{lab} = & Kin_{42} * sAPP\beta^{lab} - Kout * A\beta_{42}^{lab} - Kpl * A\beta_{42}^{lab} \\ & + Krev * A\beta_O^{lab} \end{aligned} \quad (S4.17)$$

$$\frac{d}{dt}A\beta_O^{unlab} = Kpl * A\beta_{42}^{unlab} - Krev * A\beta_O^{unlab} \quad (S4.18)$$

$$\frac{d}{dt}A\beta_O^{lab} = Kpl * A\beta_{42}^{lab} - Krev * A\beta_O^{lab} \quad (S4.19)$$

$$\frac{d}{dt}FactorX^{unlab} = Kin_x * sAPP\beta^{unlab} - Kout_x * FactorX^{unlab} \quad (S4.20)$$

$$\frac{d}{dt}FactorX^{lab} = Kin_x * sAPP\beta^{lab} - Kout_x * FactorX^{lab} \quad (S4.21)$$

The label incorporation in the APP pathway is informed from the kinetic model of plasma tracer enrichment. In Eqs. S4.8 and S4.9 this is imputed by TC_1 and TR_1 , converted from mg to pM by $10^9/MW_{Leu}$. FAC in Eqs. S4.9 is a scale correction factor, used to scale the plasma tracer enrichment to the level of tracer enrichment in the brain.

The rate of change of APP with respect to time in the presence of the inhibitor is described by Eqs. S4.8 and S4.9, in which the BACE1 cleavage inhibition is incorporated by the factor EFF . EFF is the degree of inhibition caused by MBI-5, expressed as shown in Eqs. 5.8.

$$EFF = 1 - \frac{C_{target}^{GAM} * Imax}{C_{target}^{GAM} + IC50^{GAM}} \quad (S4.22)$$

Where C_{target} is the target site concentration of MBI-5, $IC50$ the C_{target} that results in 50% inhibition of BACE1, $Imax$ is the maximum inhibition and GAM is the Hill coefficient. C_{target} was derived from the PK model as:

$$C_{target} = C_{plasma} * \frac{AUC_{CSF}}{AUC_{plasma}} \quad (S4.23)$$

Where AUC_{CSF} and AUC_{plasma} are the areas under the CSF and plasma concentration time curves, respectively. Here, C_{target} is assumed to follow the same profile as C_{plasma} , with the ratio

between the two concentrations being equal to the ratio between AUC_{CSF} and AUC_{plasma} . It is assumed that the system is in steady state when no tracer and no treatment is given ($EFF=1$). In addition, it is assumed that prior to tracer infusion, there are no labelled species. These steady state conditions were used to derive part of the system parameters.

From the steady state conditions and Eqs. S4.8 it follows that the source of APP (Rin_{APP}) was:

$$Rin_{APP} = (Rin_{\beta} + Rin_{\alpha}) * \frac{APP_{base} * MW_{LeuL}}{TC_{1base} * 10^9} \quad (S4.24)$$

Where APP_{base} is the baseline level of APP (unlabelled, prior to tracer infusion), which is assumed to be equal to the sum of the baseline levels of $sAPP_{\alpha}$ and $sAPP_{\beta}$, as all alternate pathways are represented by the terms for α -secretase. BTC_1 is the baseline of tracee pool 1.

Using the steady state conditions and Eqs. S4.10 the $sAPP_{\alpha}$ formation rate (Rin_{α}), equivalent to the α -secretase cleavage step, can be derived:

$$Rin_{\alpha} = Rout_a * \frac{sAPP_{\alpha base}}{APP_{base}} \quad (S4.25)$$

Where $sAPP_{\alpha base}$ is the baseline level of $sAPP_{\alpha}$.

The $sAPP_{\beta}$ formation rate (Rin_{β}), equivalent to the BACE1 cleavage step, follows from steady state conditions and Eqs. S4.12:

$$Rin_{\beta} = (Kin_{40} + Kin_{42} + Kin_x) * \frac{sAPP_{\beta base}}{APP_{base}} \quad (S4.26)$$

Where $sAPP_{\beta base}$ is the baseline level of $sAPP_{\beta}$.

From steady state conditions and Eqs. S4.14 the $A\beta_{40}$ formation rate (Kin_{40}), equivalent to a γ -secretase cleavage step can be calculated:

$$Kin_{40} = Kout * \frac{A\beta_{40 base}}{sAPP_{\beta base}} \quad (S4.27)$$

Where $A\beta_{40 base}$ is the baseline level of $A\beta_{40}$. $sAPP_{\beta base}$ is the baseline level of $sAPP_{\beta}$, used here as surrogate for the baseline level of C99.

From Eqs. S4.16 and steady state conditions, with substitution of $Kout$ from Eqs. S4.27, the $A\beta_{42}$ formation rate (Kin_{42}), equivalent to a γ -secretase cleavage step, is deduced:

$$Kin_{42} = Kin_{40} * \frac{A\beta_{42 base}}{A\beta_{40 base}} \quad (S4.28)$$

Where $A\beta_{42 base}$ is the baseline level of $A\beta_{42}$.

From Eqs. S4.20 and steady state conditions, the FactorX formation rate (Kin_x) is deduced:

$$Kin_x = Kout_x * \frac{FactorX_{base}}{sAPP_{\beta base}} \quad (S4.29)$$

Where $FactorX_{base}$ is the baseline level of FactorX.

The model structure includes two times six transit compartments, two for each biomarker (labelled and unlabelled) (sAPP α , sAPP β , A β 40, A β 42, A β O, FactorX), to account for transport from the target site in the brain to CSF. These transit processes are described, in general, by Eqs. S4.30 and S4.31:

$$\frac{d}{dt} \text{species}_{CSF}^{lab} = Kt * (\text{species}^{lab} - \text{species}_{CSF}^{lab}) \quad (S4.30)$$

$$\frac{d}{dt} \text{species}_{CSF}^{unlab} = Kt * (\text{species}^{unlab} - \text{species}_{CSF}^{unlab}) \quad (S4.31)$$

Where Kt is the transit rate for the particular species ($KtAP$ for sAPP α and sAPP β ; $KtAB$ for A β 40, A β 42 and A β O; KtX for FactorX).

The fraction labelled species (FracLab) for each APP metabolite in CSF are calculated as labelled over total species (Eq. S4.32-S4.34).

$$\text{FracLab}_{sAPP\alpha_{CSF}} = \frac{sAPP\alpha_{CSF}^{lab}}{sAPP\alpha_{CSF}^{Total}} \quad (S4.32)$$

$$\text{FracLab}_{sAPP\beta_{CSF}} = \frac{sAPP\beta_{CSF}^{lab}}{sAPP\beta_{CSF}^{Total}} \quad (S4.33)$$

$$\text{FracLab}_{A\beta_{CSF}} = \frac{A\beta_{40CSF}^{lab} + A\beta_{42CSF}^{lab} + A\beta_{O_{CSF}}^{lab} + \text{FactorX}_{CSF}^{lab}}{A\beta_{40CSF}^{Total} + A\beta_{42CSF}^{Total} + A\beta_{O_{CSF}}^{Total} + \text{FactorX}_{CSF}^{Total}} \quad (S4.34)$$

The total concentrations for each APP fragment in CSF are calculated as:

$$\text{Total}_{\text{species}_{CSF}} = \text{species}_{CSF}^{lab} + \text{species}_{CSF}^{unlab} \quad (S4.35)$$